

# Hydromechanics, biophysics of blood and respiration

# Properties of gas and liquid

- Mechanics of fluid
  - Aeromechanics
    - Aerostatics
    - Aerodynamics
  - Hydromechanics
    - Hydrostatics
    - hydrodynamics

# Gas properties

- Do not have their own shape and volume
- Compressible
- $E_k > E_p$
- Convective heat transfer
- Gas leads electric current under certain conditions

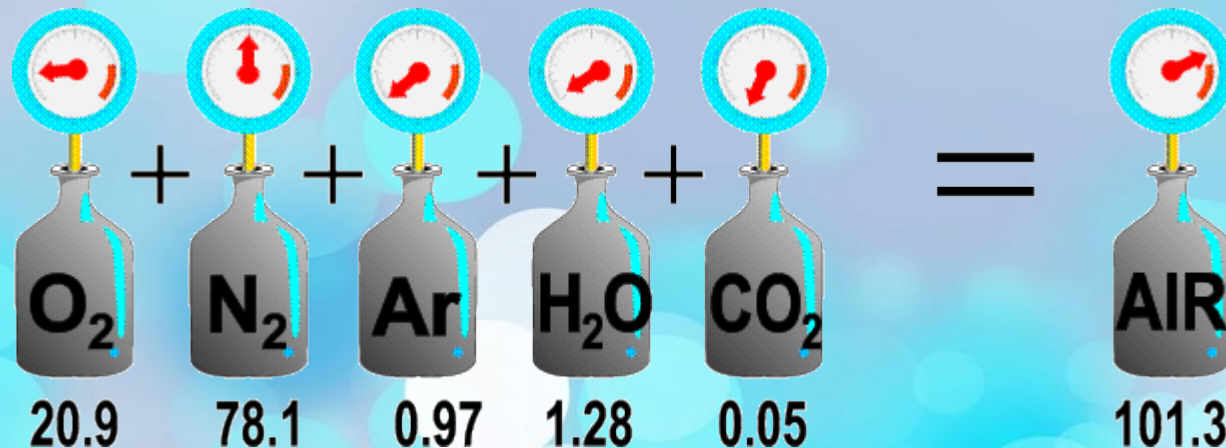
# Gas properties

- Gas volume
  - At 0 °C and 101 325 Pa volume of 1 mol is equal to 22,414 dm<sup>3</sup>
  - IUPAC conditions: at 0 °C and 100 000 Pa volume of 1 mol is equal to 22,71 dm<sup>3</sup>

# Gas properties

- Dalton's Law
  - In a mixture of non-reacting gases, total pressure of the gaseous mixture is equal to the sum of partial pressures of individual gases.

$$P = p_1 + p_2 + p_3 + \dots + p_n$$

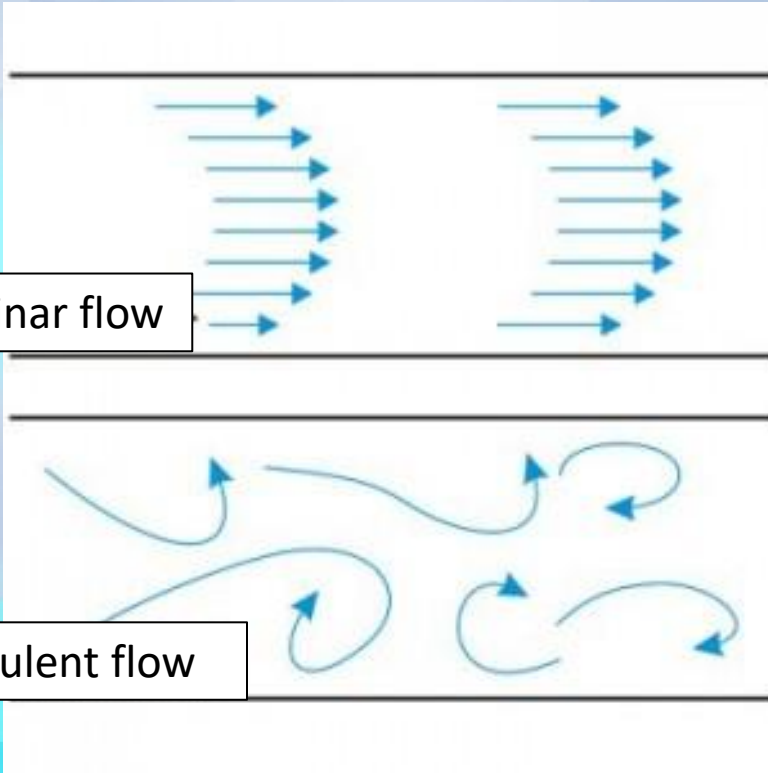




# Gas properties

- Air flow

Laminar flow



Turbulent flow



# **Respiration biophysics**

# Respiration

- Intake of  $O_2$  to tissue and dispose of  $CO_2$  from organism
- External respiration
  - Gas exchange between alveolar gas and blood
- Internal respiration
  - Gas exchange between blood and tissue



# External respiration

1. Pulmonary ventilation
2. Distribution
3. Diffusion
4. Perfusion

# 1. Pulmonary ventilation

- Inspiration – active action; contraction of respiration muscles (diaphragm)
  - Pressure gradient to lungs; air is drawn in
  - Action happens against resistance
    - Elasticity of pulmonary tissue
    - Surface tension of alveoli (Laplace law)
    - Inelastic tissue resistance (= tissue viscous resistance) - friction of lung tissue, chest, respiratory muscles etc.
    - Flow resistance of the airways - a summary of several types of resistances, caused by the airways (turbulence, viscosity...)

# 1. Pulmonary ventilation

- Expiration – passive action
  - Pressure gradient from lungs to the outside; air is expelled
  - Happens spontaneously
    - Tissue flexibility
    - Muscle relaxation
  - Muscles work in forced expiratory

# Respiration mechanics

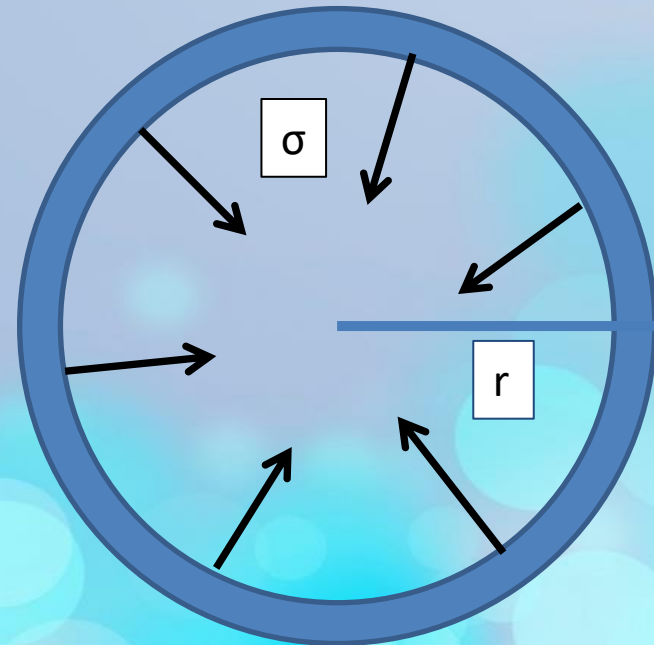
- Lungs and chest elasticity
  - Creates retraction force = tendency to lower volume
  - Extension of lungs is conditioned with pressure increase
  - Lungs pliability – Lungs compliance
    - Static x dynamic (continual record)

$$E = \frac{\Delta p}{\Delta V} \quad c = \frac{\Delta V}{\Delta p}$$

# Respiration mechanics

- Retraction force of lungs
  - Its influence leads to decrease of alveoli diameter during expiration
  - Laplace's law:

$$p = \frac{2\sigma}{r}$$





# Respiration mechanics

- Negative pleural pressure
  - Pressure in area between pleuras
    - Inspiration: - 0,8kPa
    - Expiration: - 0,33 kPa
  - Lymphatic system constantly sucks in pleural liquid
  - Lungs are distended, they follow movement of respiration muscles
  - damage = pneumothorax – lung collapse

## 2. Distribution

- Intake of air to lungs and its mixing with air, which was left in lungs after last expiration
- Dead space – volume of airways, where exchange of gases is not happening (150 ml)

# 3. Diffusion

- movement of gases through alveolar membrane in the direction of concentration gradient (from location with high concentration to location with lower concentration)
- Description of diffusion: Adolf Fick -> Fick's diffusion laws

# 3. Diffusion

- 1. Fick's law
  - Diffusion flux is directly proportional to substance concentration (calm state)

$$J = -D \frac{\Delta C}{\Delta X}$$

$$\frac{n}{S.t} = -D \frac{\Delta C}{\Delta X}$$

J ... diffusion flux [mol.m<sup>-2</sup>.s<sup>-1</sup>]

n ... amount of substance [mol]

x ... distance [m]

t ... time [s]

D ... diffusion coefficient [m<sup>2</sup>.s<sup>-1</sup>]

c ... concentration [mol.m<sup>-3</sup>]

S ... cross-section area [m<sup>2</sup>]

# 3. Diffusion

- Gas diffusion speed through alveocapillary membrane

- derived from Fick's law

$$V / t = \frac{(P_1 - P_2) \cdot S \cdot k}{d}$$

- k = diffusion constant (directly proportional to solubility coefficient alpha, inversely proportional to square root of molecular weight)

$$k = \frac{\alpha}{\sqrt{m_h}}$$



# 3. Diffusion

- Amount of gas dissolved in liquid medium=  
Henry's law
  - Amount of dissolved gas is directly proportional to partial pressure of gas above the liquid medium and its solubility coefficient

$$V = \frac{\alpha \cdot p_t \cdot 1000}{P_B}$$

V ... volume

P<sub>t</sub> ... partial gas pressure

α ... solubility coefficient

P<sub>B</sub> ... total barometric pressure

# 3. Diffusion

- Solubility coefficient alpha
  - Gas amount dissolved in 1 ml of liquid at 0 °C temperature and pressure 101,3 kPa
  - Human body  $t = 37\text{ °C}$

# 3. Diffusion

**O<sub>2</sub>**

98.6% bound to hemoglobin

1.4% physically dissolved

**CO<sub>2</sub>**

20 times more soluble than O<sub>2</sub>; 46 times more soluble than N<sub>2</sub>

94% chemically bound as HCO<sub>3</sub><sup>-</sup> CO<sub>3</sub><sup>2-</sup>

6% physically dissolved

**N<sub>2</sub>**

100% physically dissolved (inert gas)

More soluble in adipose tissue

# 4. Perfusion

- Permanent perfusion of pulmonary tissue
  - Rich perfusion, including alveoli surrounded by capillaries, helps to maintain pressure gradient of gases

# Decompression syndrome

- Equalization of partial pressures is performed by diffusion
- $N_2$  more soluble in fat tissue than in blood
- Equalization of  $N_2$  pressures is slower
- During quick decompression diffusion is not enough to equalize
- Creation of air bubbles
- Bubbles can cause emboly



# Decompression syndrome

- Pressure chamber (barochamber)
  - Oxygen overpressure
  - Burns
  - CO<sub>2</sub> poisoning
  - Shock state



# Altitude sickness

Atmospheric pressure reduction

- at normal barometric pressure

$$p_{i O_2} = 21.3 \text{ kPa}$$

- at an altitude of 4,000 m

$$p_{i O_2} = 13.3 \text{ kPa}$$

- Reduction of oxygen saturation
- Altitude hypoxia
- Compensation

# Properties of liquids

- Do not have a shape
- Do have a volume
- Form surface
- Hardly compressible
- Convective heat transfer
- With presence of ions = el. current conductive

# Hydromechanics

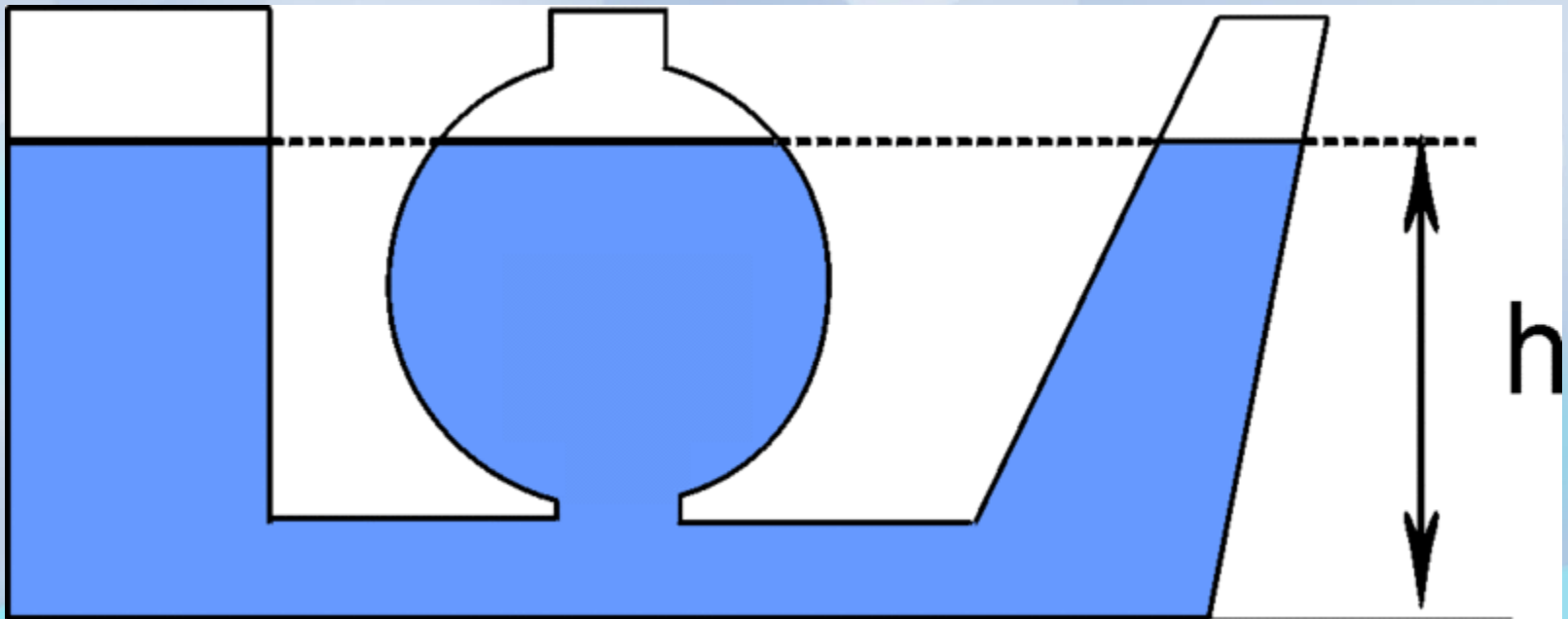
- Studies physical behavior of liquids
- a) hydrostatics – behavior of liquids at rest
- b) hydrodynamics - behavior of liquids in motion

# Hydromechanics

- The hydrostatic pressure  $p_h = h \cdot \rho \cdot g$  the pressure caused by the weight of the liquid on a body immersed in a certain depth (or at the vessel wall, but also to itself); caused by the gravitational force
- Hydrostatic force  $F_h = p_h S (h \cdot \rho \cdot g \cdot S)$ 
  - compressive force by which the liquid pushes at the immersed body at a certain depth (or. at the vessel wall, but also to itself)



# Communicating vessels



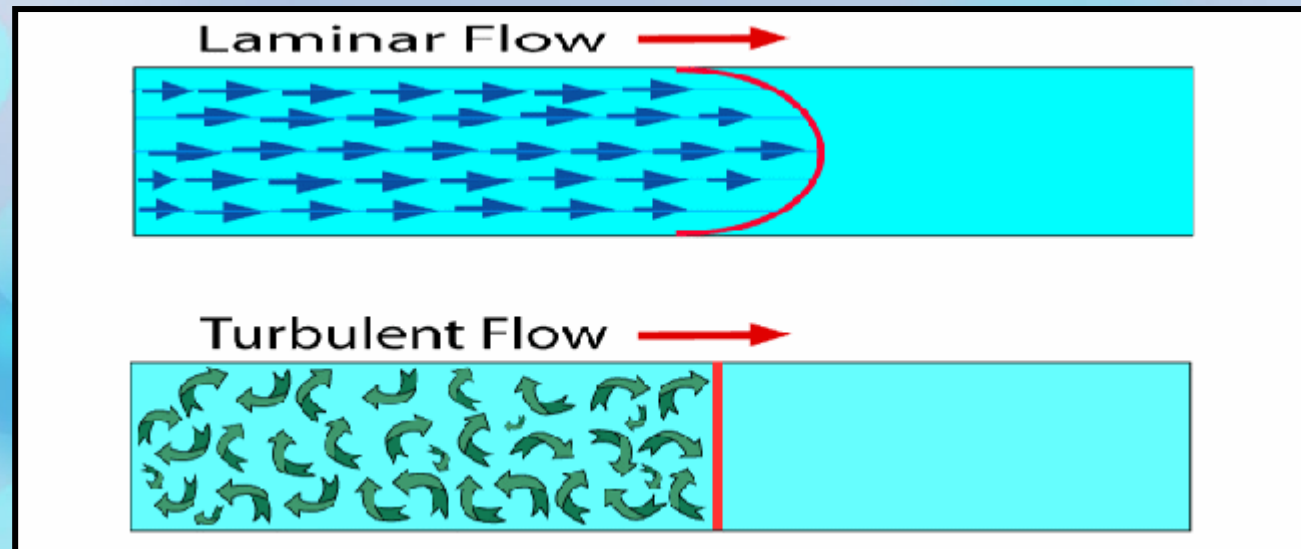
# Hydrodynamics

## Liquid flow

- Fluid movement, wherein the liquid particles move by disordered movement and by the movement in the flow direction
- Fluid flowing from higher pressure to areas of low pressure
- The trajectory of particles = streamline  
Stationary x nonstationary flow

# Hydrodynamics

- The flow of viscous liquids
  - Laminar – streamlines are parallel
  - Turbulent – streamlines are random, mingled, nonstationary movement

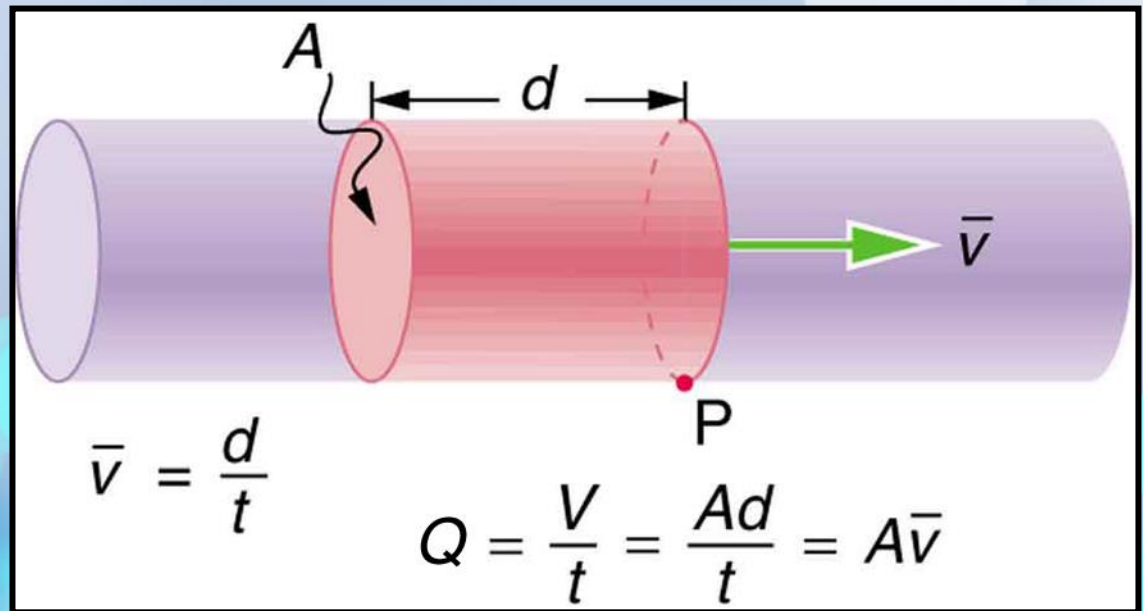


# Volume flow rate

- Liquid volume, which flows through cross-section per time unit

$$Q_v = \frac{\Delta V}{\Delta t}$$

$$Q_v = S \cdot v$$



# Hydrodynamics

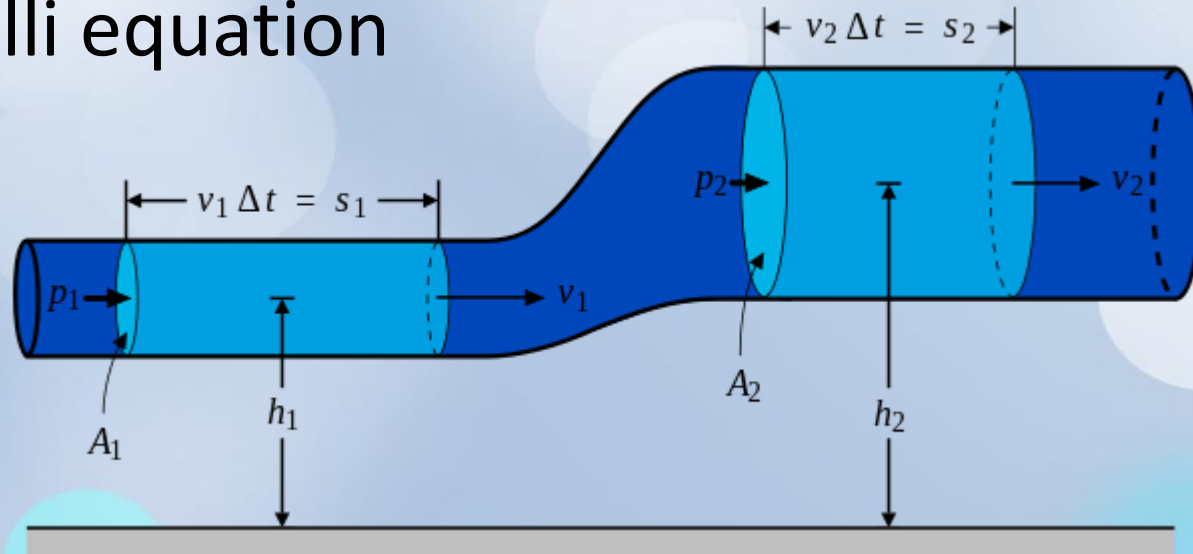
- Bernoulli equation
- The law of energy conservation for a stable flow of ideal fluid
  - The sum of the potential pressure energy, kinetic energy, and potential energy is constant

$$\frac{1}{2} \cdot \rho \cdot v^2 + h \cdot \rho \cdot g + P = \textit{const.}$$



# Hydrodynamics

- Bernoulli equation



- In the place with a larger cross-section the flowing liquid has higher pressure, but lower speed, in a place with a smaller cross-sectional area has a smaller pressure but greater speed = pressure decreases with increasing speed

# **Biophysics of blood circulation**

# Biophysics of blood circulation

- Circulatory system

- Heart
- Vessels
- Blood

- Vessels – arteries, capillaries, veins

They have the possibility of some volumetric expansion (of elasticity), which is given by the coefficient of volumetric expansion  $E$ :

$$E = \frac{\Delta p}{\Delta V}$$

$$c = \frac{\Delta V}{\Delta p}$$

# Biophysics of blood circulation

## Vascular system

### Arterial part

- Arteries, arterioles, metarterioles
  - The aorta and arteries have great content of elastic tissue  
=> elastic effect => pulse
  - The heart works discontinuously, but pulsation is unsuitable for proper diffusion in tissues
    - elastic arterioles - similar to arteries and aorta = high content of elastic fibers - expand in systole
    - muscular arterioles - a high content of smooth muscle fibers - maintain pressure during diastole
- = alternating both types of arterioles removes or at least minimizes the effect of pulsation in the capillaries, where a pressure of a constant value is then present

# Biophysics of blood circulation

## Capillary part

- It provides exchange between the arterial circulation and tissues
- Diffusion - is carried out through the pores of the capillary membranes (water-soluble substances) or whole capillary membrane (lipid-soluble substances; phenomenon describes the first Fick law)

$$J = -D \frac{\Delta c}{\Delta x}$$

J ... diffusion flux [ $\text{mol} \cdot \text{m}^{-2} \cdot \text{s}^{-1}$ ]  
n ... amount of substance [mol]  
x ... distance [m]  
t ... time [s]

$$\frac{\Delta n}{S \cdot \Delta t} = -D \frac{\Delta c}{\Delta x}$$

D ... diffusion coefficient [ $\text{m}^2 \cdot \text{s}^{-1}$ ]  
c ... concentration [ $\text{mol} \cdot \text{m}^{-3}$ ]  
S ... cross-section area [ $\text{m}^2$ ]



# Biophysics of blood circulation

## Capillary part

- It provides exchange happening between the arterial circulation and tissues
  - Filtration – depends on hydrostatic and colloid osmotic pressure; filtered volume is given by formula:

$$V = K \cdot (p_k - \pi_k + \pi_{iF} - p_{iF})$$

$K$ ... filtration coefficient

$p_k$ ...blood pressure

$p_{iF}$ ...interstitial fluid pressure

$\pi_k$ ...col. osm. blood press.

$\pi_{iF}$ ...col. osm. int. fl. press.

# Biophysics of blood circulation

- Venous part
  - Less elastic, less muscle
  - In venous return: valves, the muscles of the lower limbs, the negative pressure in the pleural cavity are involved

# Blood

- Blood plasma – a colloidal solution; viscoelastic fluid
  - Blood cells
    - Red blood cells - adhesion at a slower flow rate
- = suspension system

# Blood

- Blood viscosity – viscosity characterizes internal friction in liquid, it depends on the attractive forces between the particles, viscosity indicates the ratio between shear stress and speed in dependency on the distance between adjacent layers

– Dynamic viscosity

$$\eta = \frac{F}{S} \cdot \frac{\Delta x}{\Delta v} \quad \text{Pa.s}$$

Kinematic viscosity

$$\nu = \frac{\eta}{\rho} \quad \text{Stokes}$$

# Blood

Blood viscosity:  $\eta_s = \eta \cdot (1 + k \cdot c)$   
(suspension)

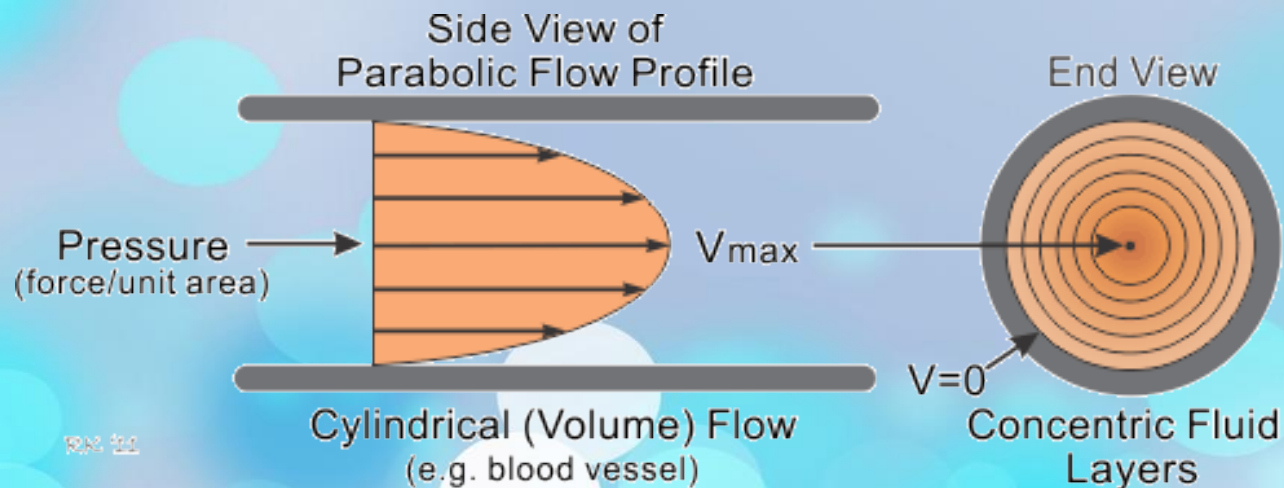
$\eta$  is fluid viscosity without solid phase,  $k$  is a constant characterizing solid particles properties,  $c$  is volume concentration of particles

Blood viscosity depends on temperature:  
for 37 °C approx  $3 - 3,5 \cdot 10^{-3} \text{ Pa} \cdot \text{s}$   
Clinically = blood sedimentation



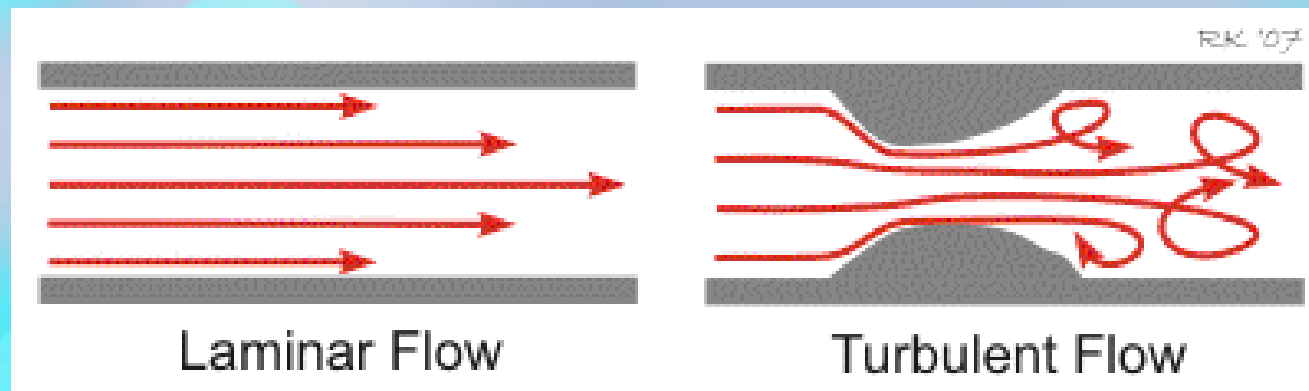
# Blood flow

- Physiologically, blood flow is laminar flow, liquid layer at vessel wall is the slowest moving layer, speed of blood flow is increasing in direction towards the center of the vessel



# Blood flow

- Patophysiologically, turbulent flow is formed in places, where vessels are obstructed, or in vessel with lowered lumen – increase of flowing speed => creation of turbulent flow; heart murmur



# Reynolds number

- Flow of liquid is laminar just to a certain value of speed – critical speed – then the flow becomes turbulent; threshold is determined by Reynolds number

$$R = \frac{\rho d v}{\eta}$$

- Laminar/turbulent borderline
- $2320 < R < 4000$
- Blood = 1000