

Lecture 8

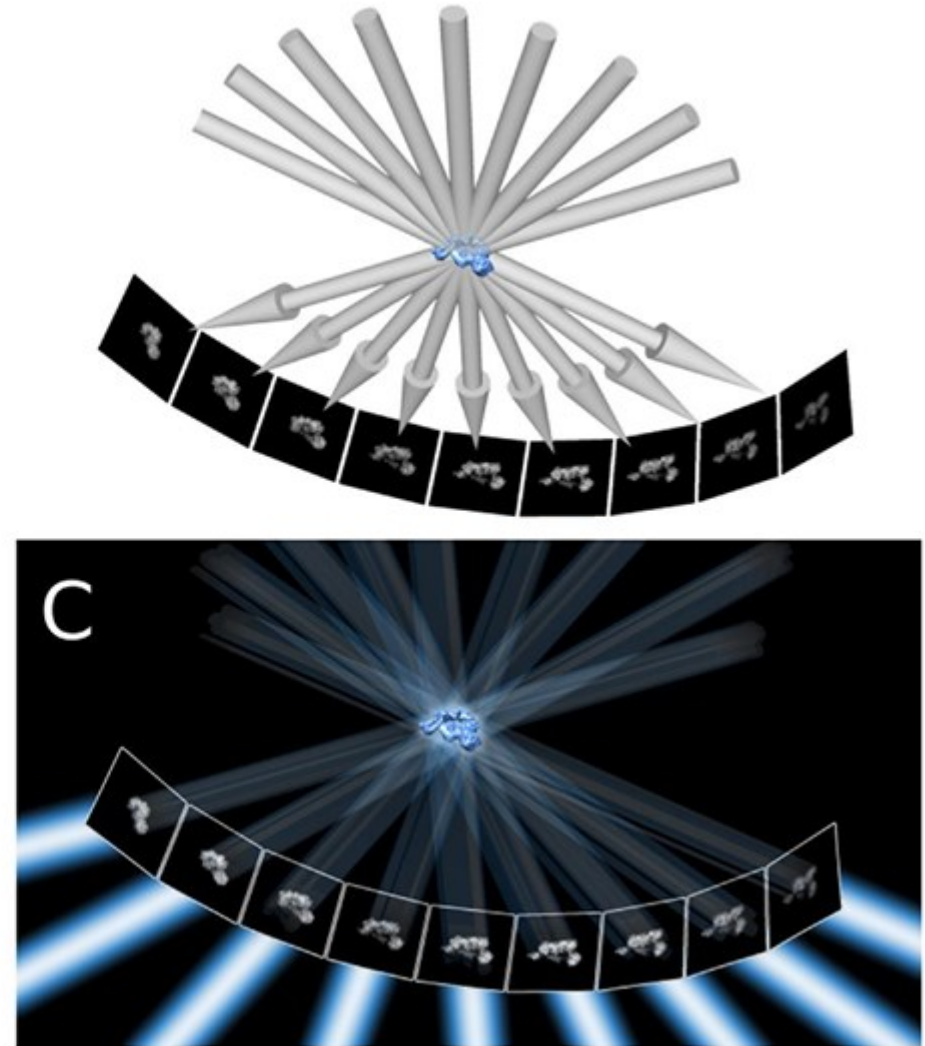
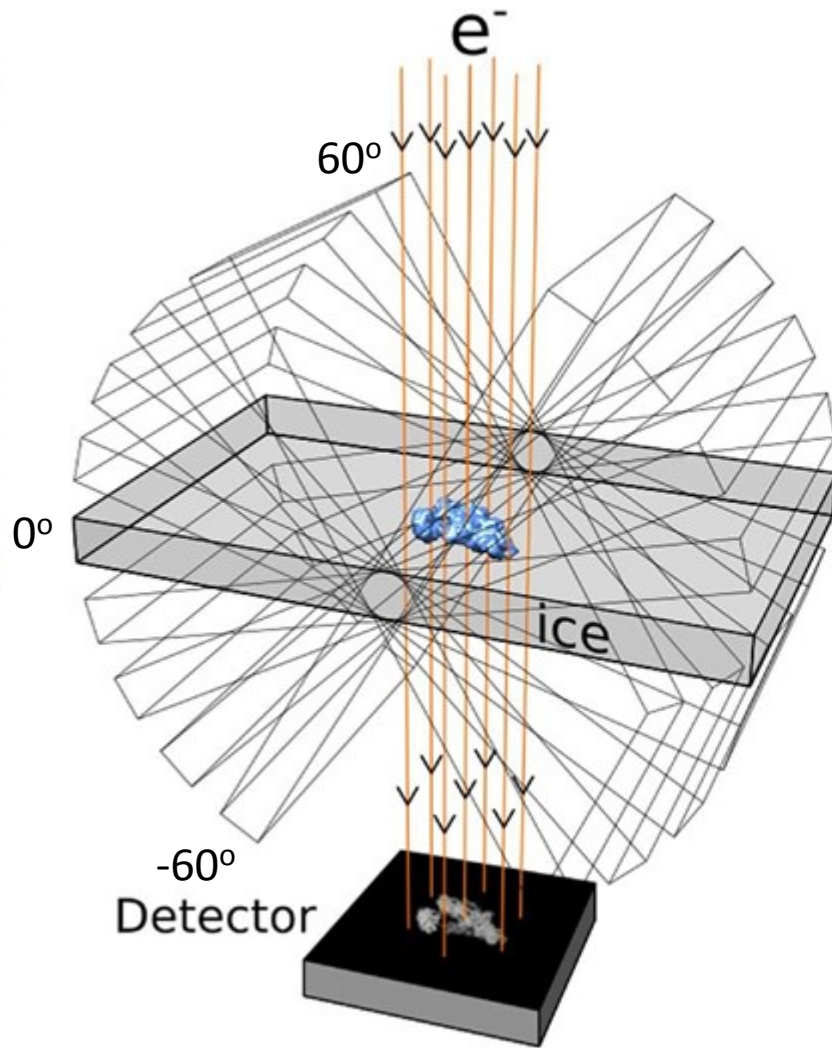
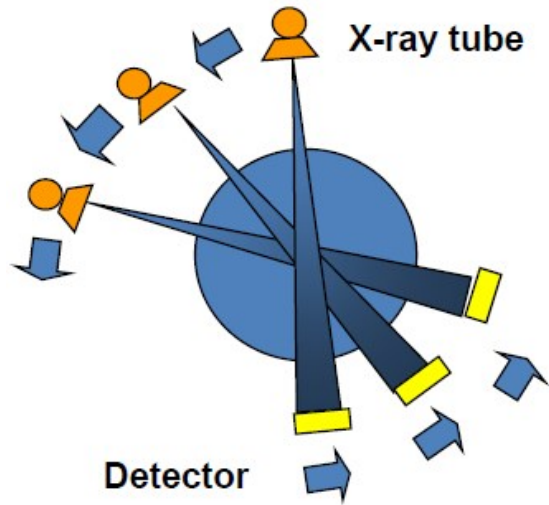
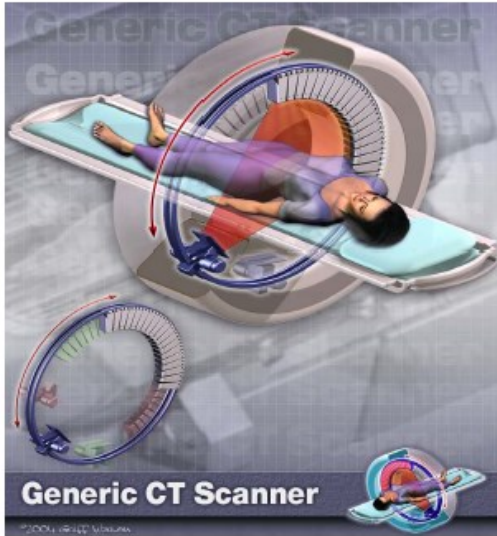
3DEM methods

Electron tomography

Tibor Füzik

Electron tomography

Computer Tomography



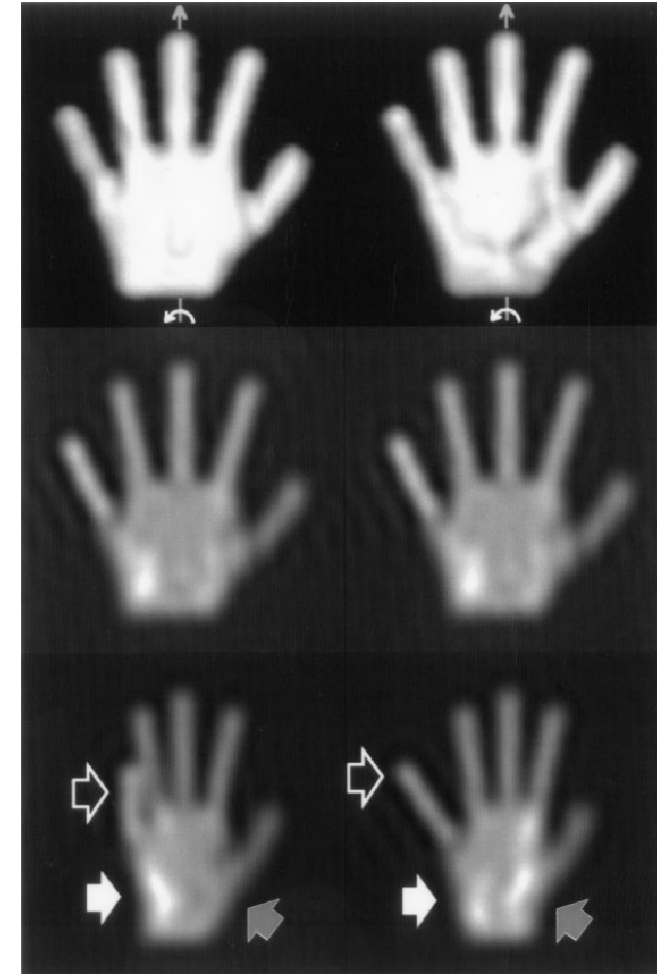
Tomography vs Single particle analysis

- **Single particle analysis**

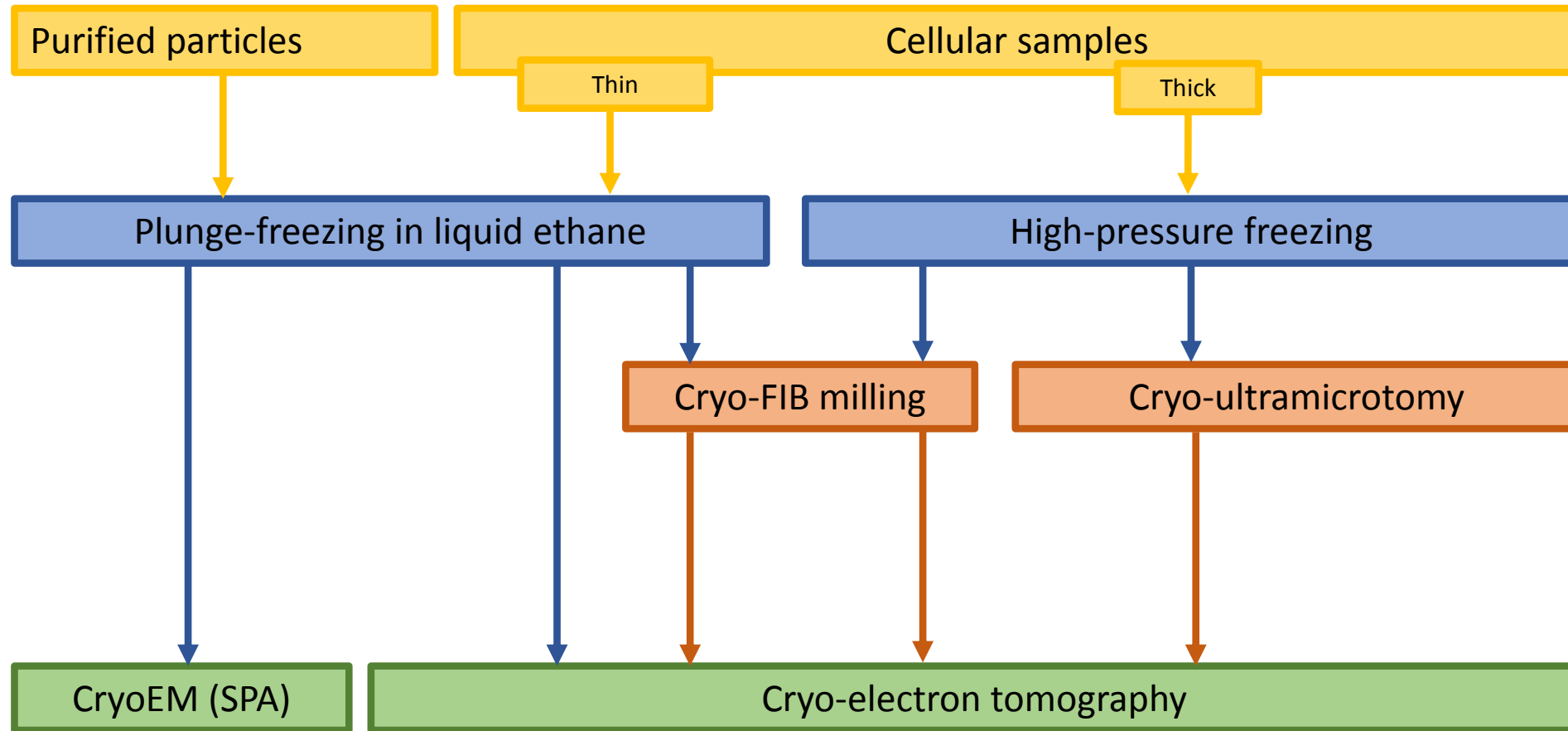
- Taking single projection image of the sample
- Exposing the acquisition area only once (“high” SNR)
- Assuming that the object of interest is in random uniform orientations
- Cannot make 3D reconstruction from a single 2D projection
- Not suitable for samples where 3D information from single acquisition area is needed (cells, non-uniformly organized structures)
- Sample needs to be electron transparent

- **Tomography analysis**

- Taking multiple projection images of the same area under different tilts
- Exposing the acquisition area multiple times (low dose, low SNR)
- Tilt angles can be assigned to the projection images
- From series of tilts, we can reconstruct a 3D volume
- Suitable for studying large samples, macromolecules *in situ*, poorly organized structures
- No ambiguity in handedness determination
- Sample needs to be electron transparent

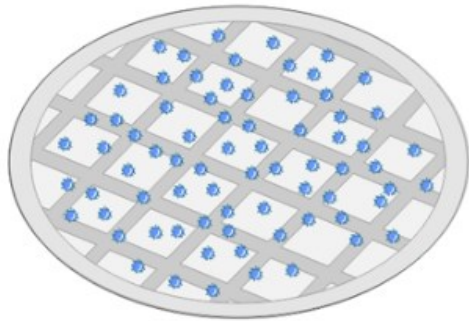


Sample preparation for tomography

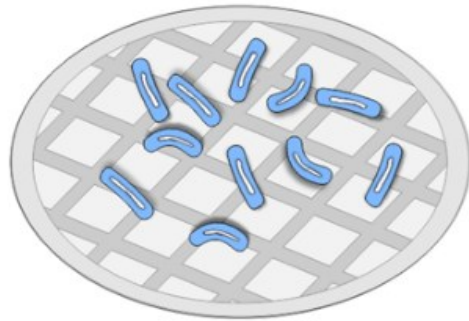
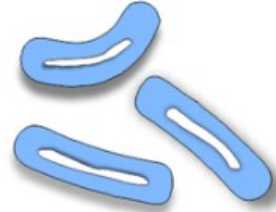


Sample preparation for tomography

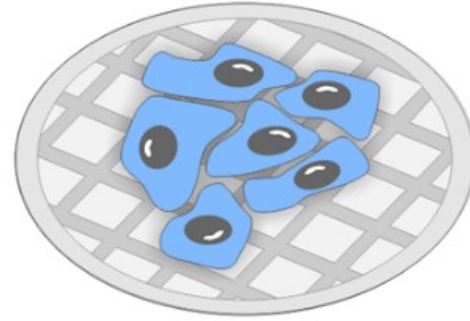
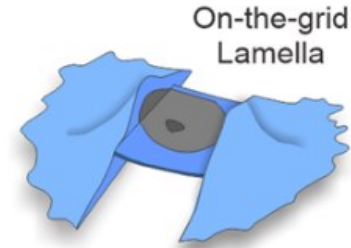
PROTEINS
VIRUSES



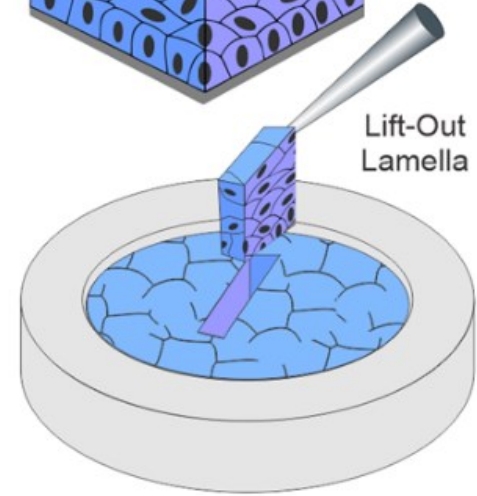
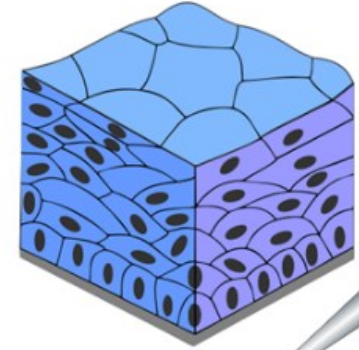
BACTERIA



CELLS



TISSUE CELLS



Plunge Freezing

High-Pressure Freezing

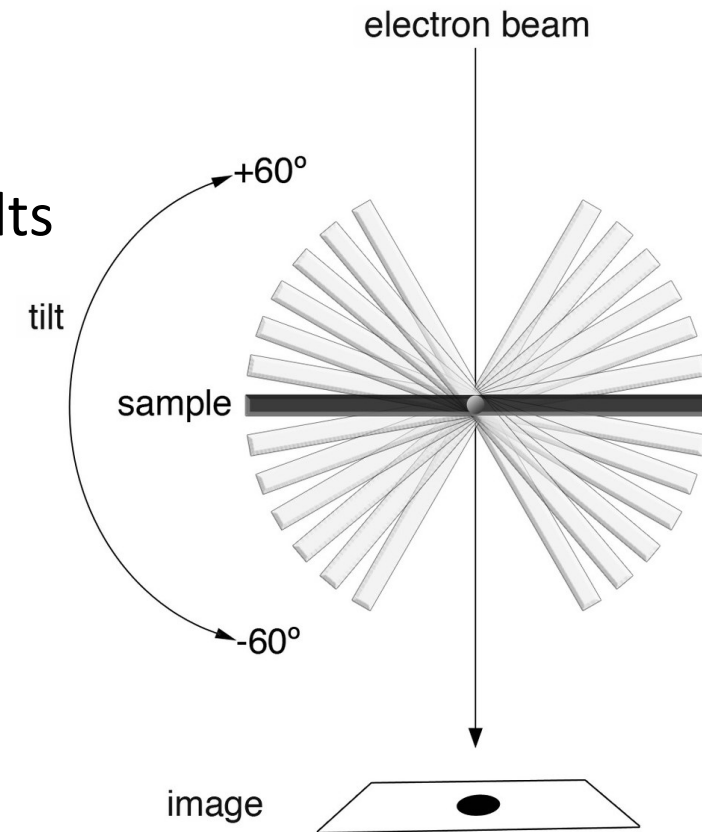
No Thinning

Cryo-FIB

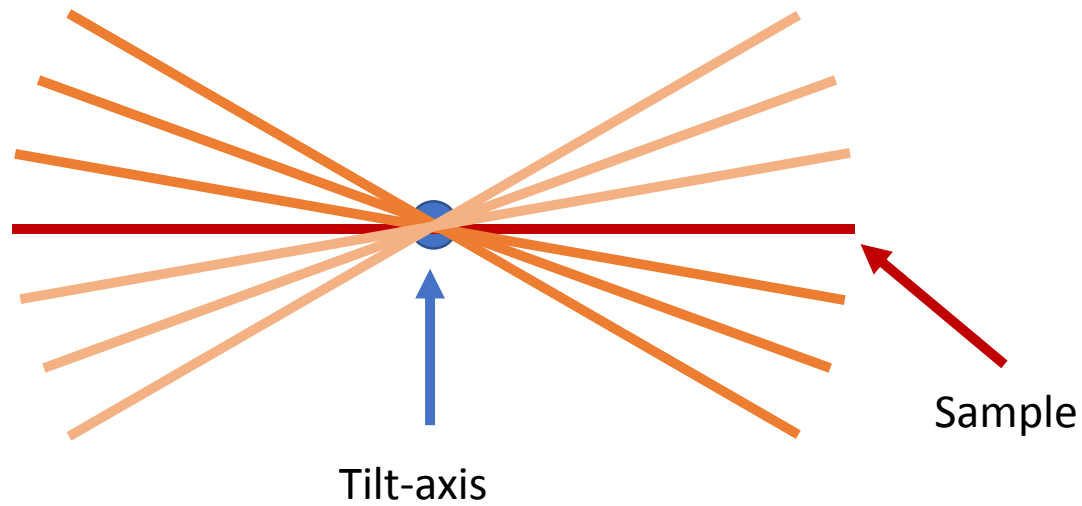
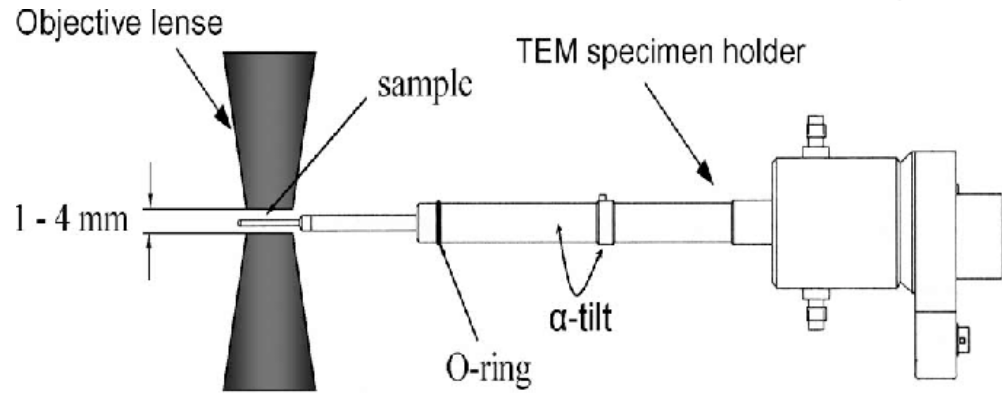
Cryo-Lift-Out

Acquisition

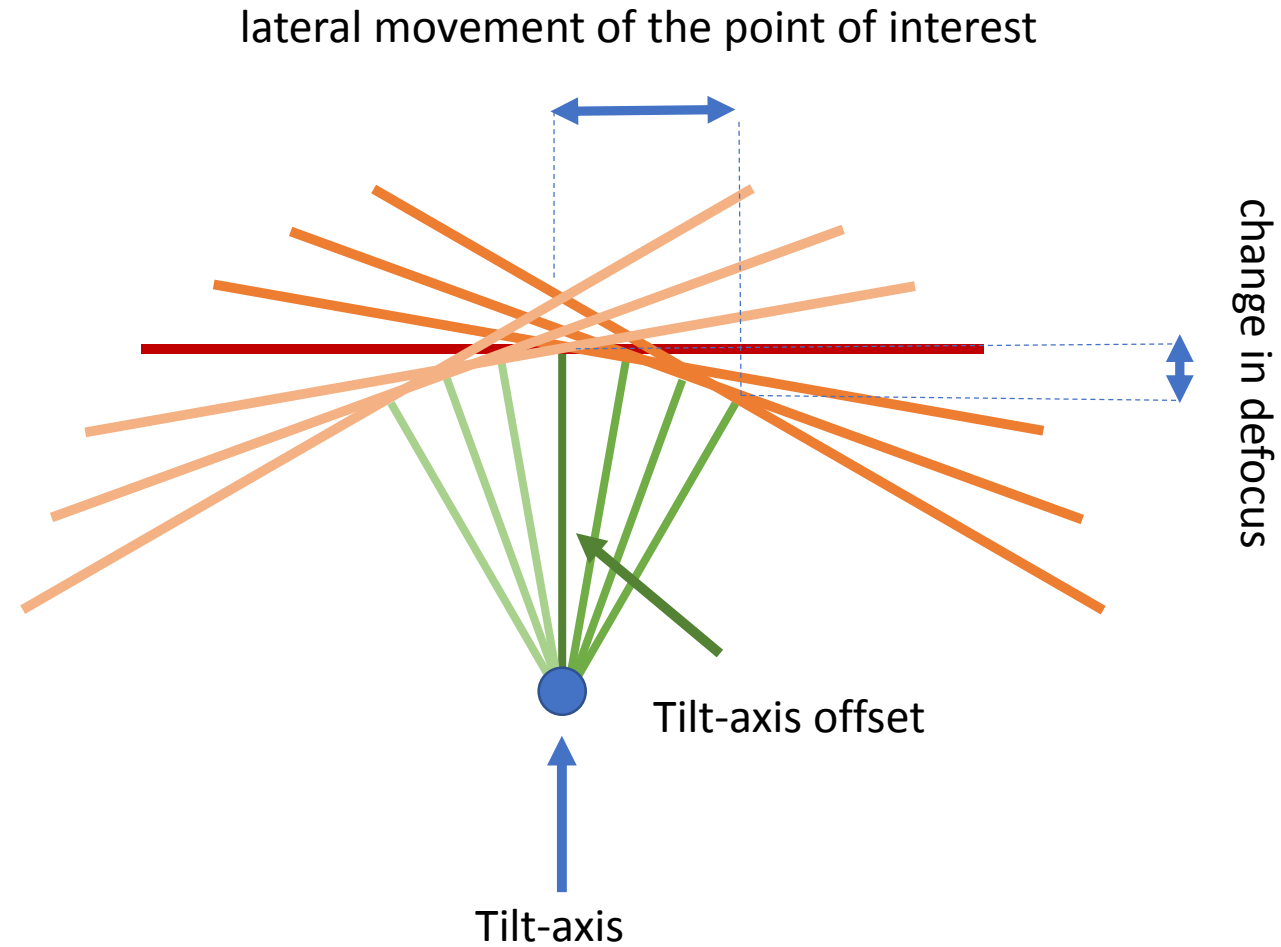
- Acquisition of tilt-series
 - Single acquisition area exposed multiple times
- Radiation damage
 - Electron dose per tilt $\sim 2-3 \text{ e-}/\text{\AA}^2$
 - Total electron dose = number of tilts * dose per tilt ($100-150 \text{ e-}/\text{\AA}^2$)
 - Dose symmetric tilt scheme
- Inclusion of fiducials in the sample
 - Small (5-10 nm) gold beads allowing precise tracking of the tilts
- Defocus during tilt-series
 - Usually kept constant
- Proper alignment of tilt axis
 - Set of eucentric height (center of rotation)
 - Corrections



Correct eucentric height – no tilt axis offset



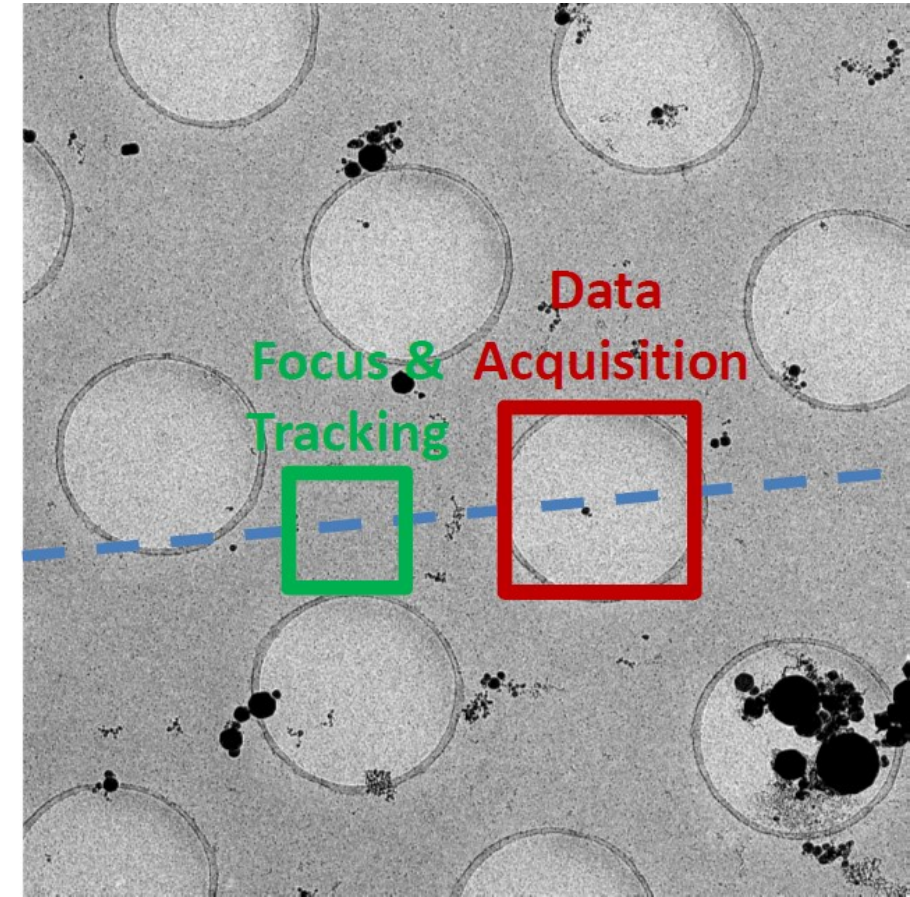
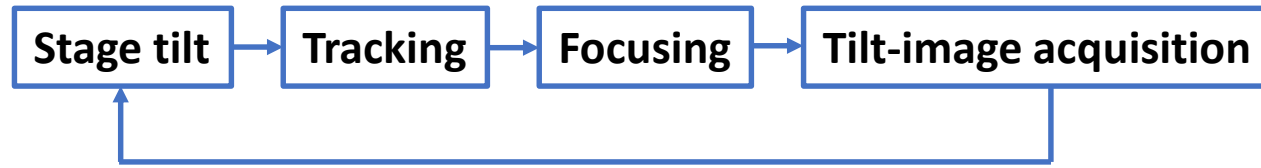
Zero tilt-axis offset



Non-zero tilt-axis offset

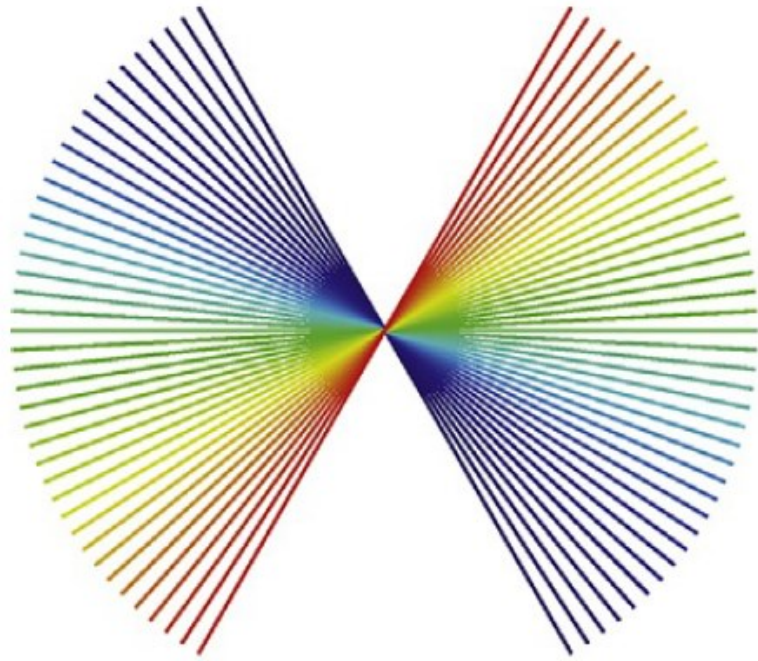
Compensation for tilt-axis offset

- After each tilt change a “tracking area” is imaged and by cross correlation with the previous image correction to image shift is done
- After each tilt change autofocus is done on focusing area
- Tracking and focusing area **must** lay on the tilt-axis



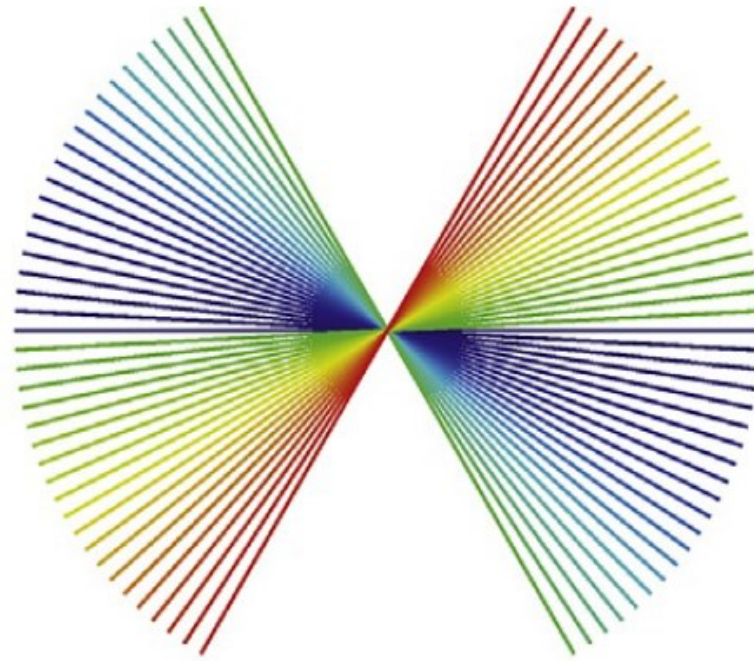
Tilt schemes

- Order in which the tilts are collected



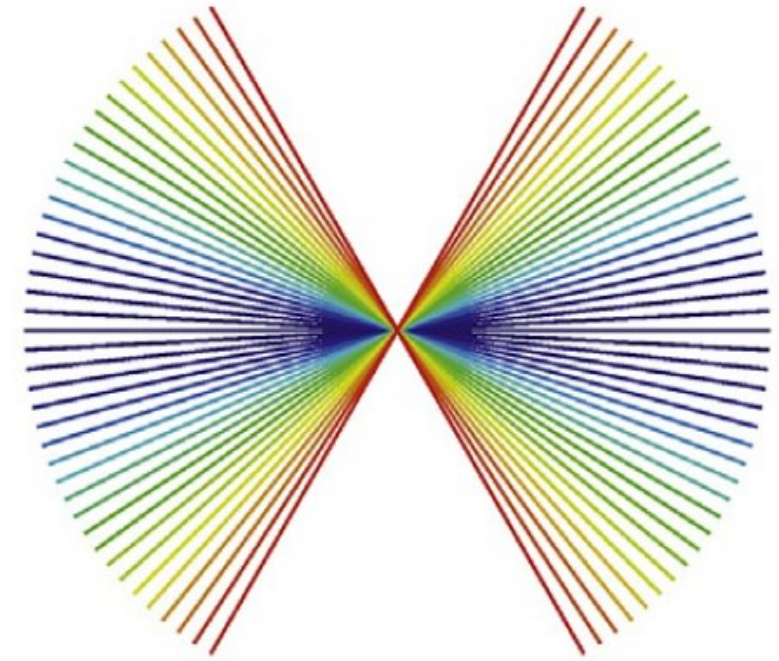
Unidirectional tilt scheme

From most positive
to most negative tilt
 $60^\circ \rightarrow -60^\circ$



Bidirectional tilt scheme

From zero to most positive
From zero to most negative tilt
 $0^\circ \rightarrow 60^\circ$; $0^\circ \rightarrow -60^\circ$



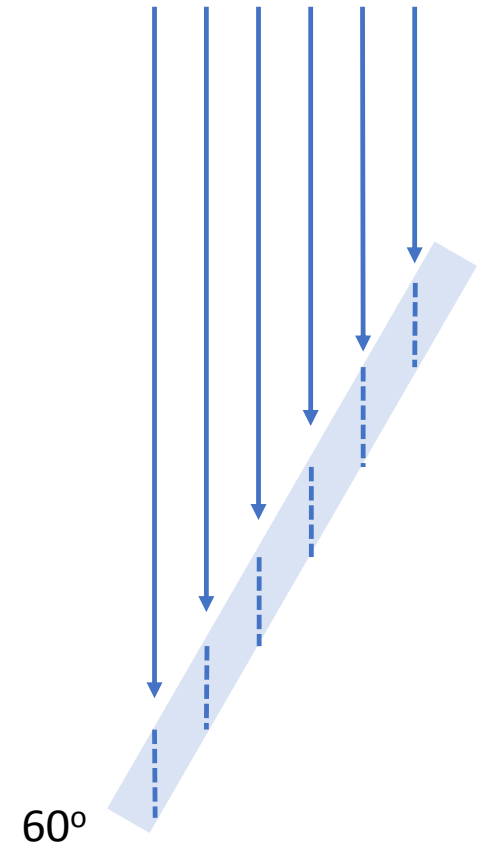
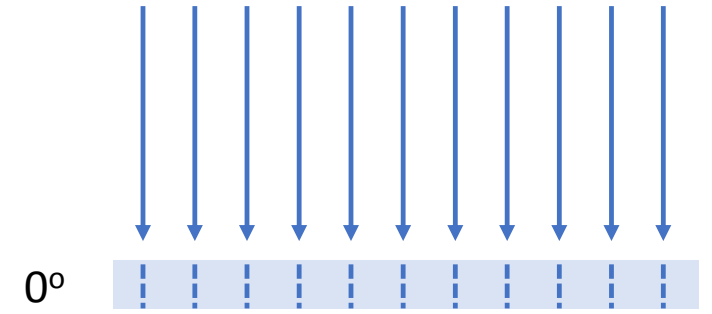
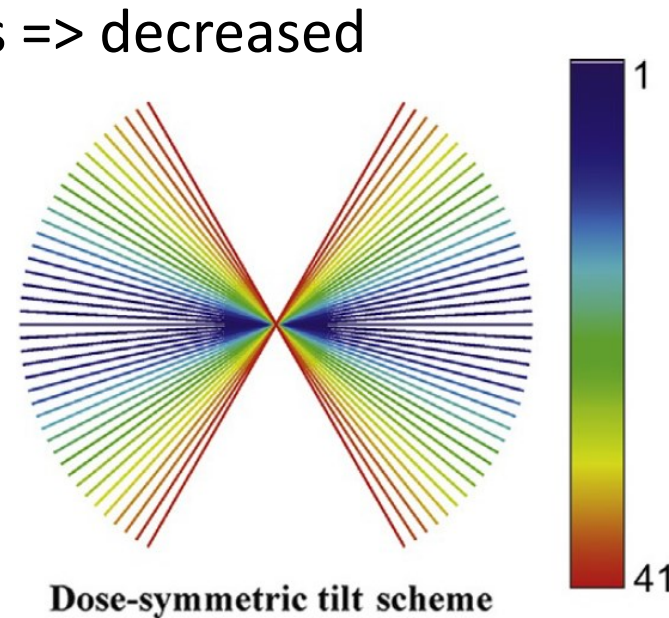
Dose-symmetric tilt scheme

Positive, positive, negative, negative,
positive, positive, negative, negative,
 $0, 3; -3, -6; 6, 9; -9, -12; 12, 15; -15 \dots$

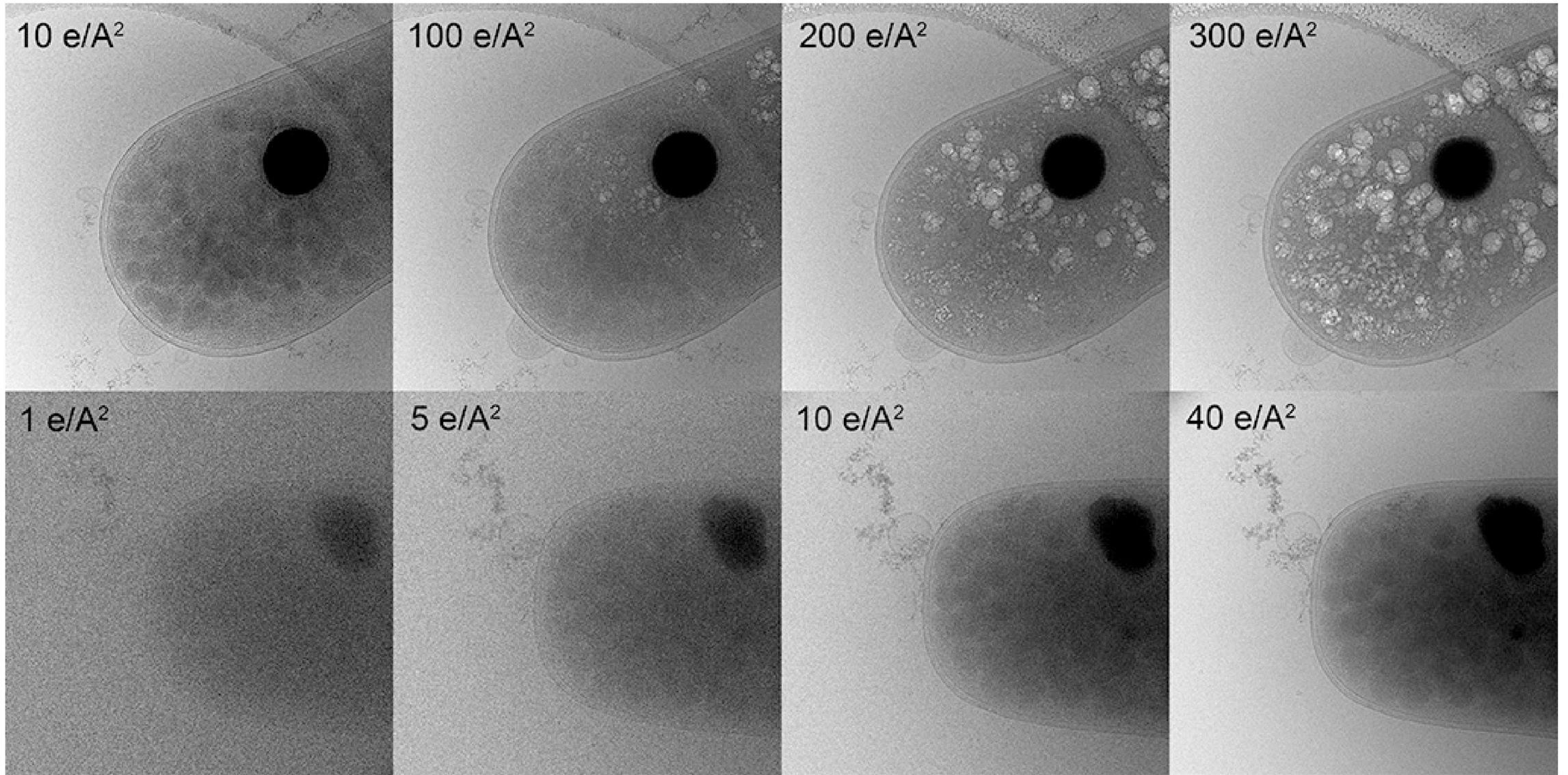


Dose symmetric tilt-scheme

- First the small angle tilts are collected
 - Sample thickness is minimal => most transparent part
 - High contrast
 - Lower radiation damage
 - Contain the most useful high freq. information
- Last the high angle tilts are collected
 - Tilt-induced grow in sample thickness => decreased transparency
 - Lower contrast
 - Higher radiation damage



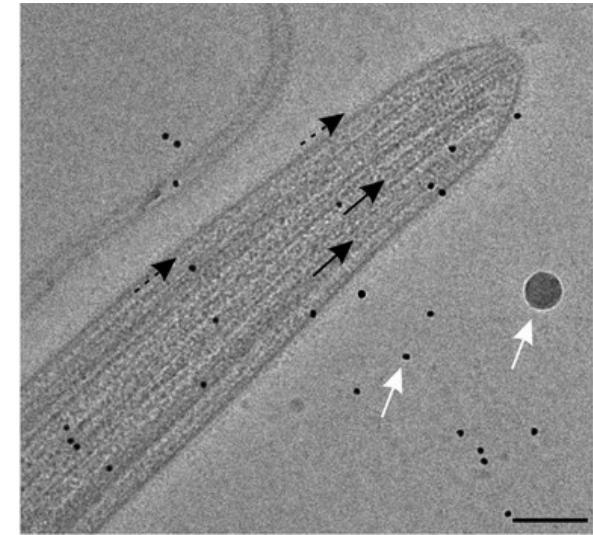
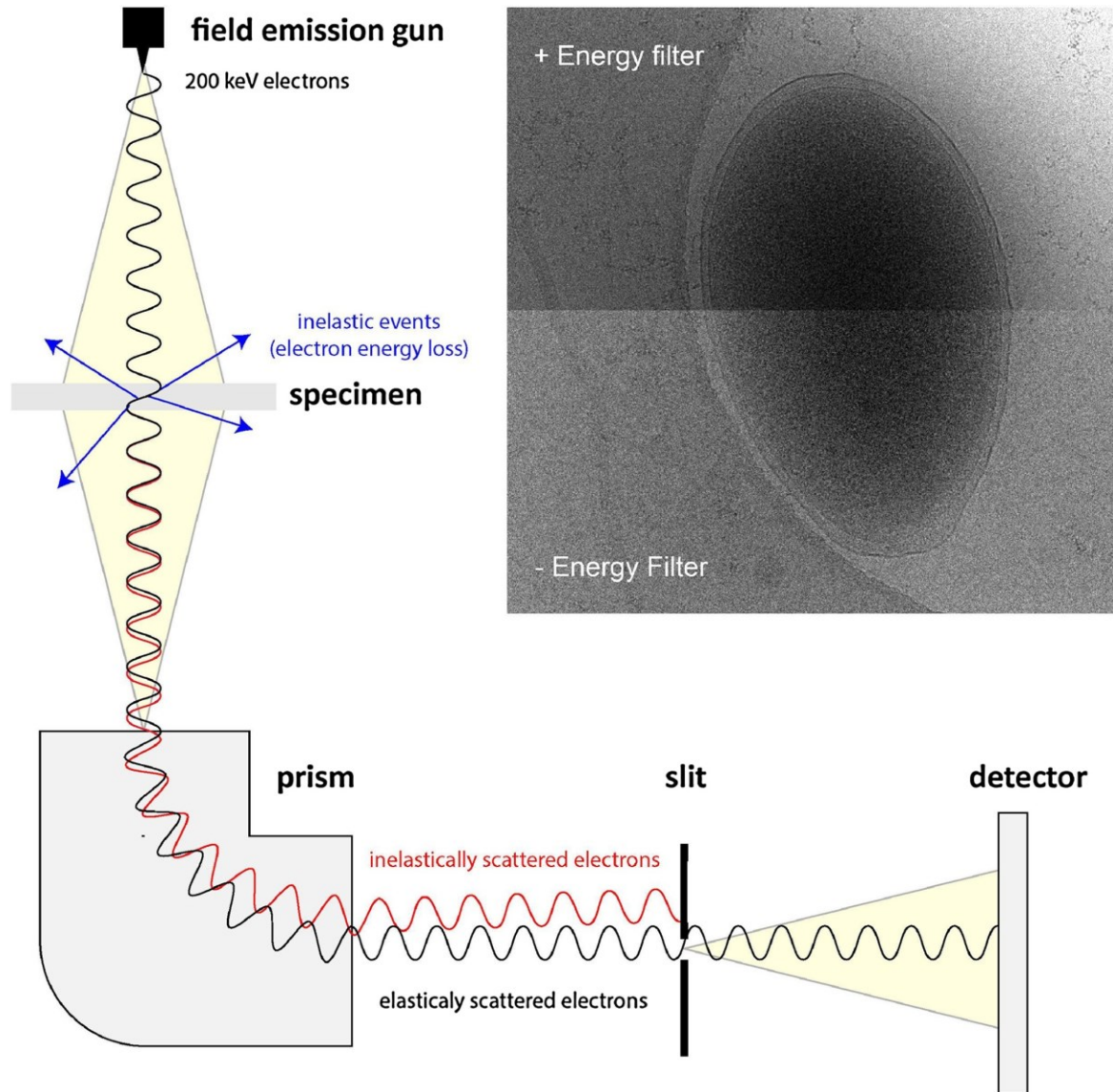
Radiation damage of cellular samples



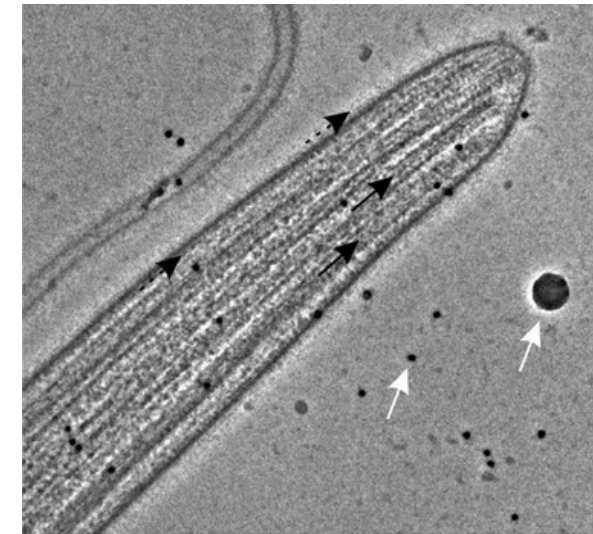
Acquisition setup

- Stage setup
 - Choice of angular increment / max tilt angle (e.g. $\pm 60^\circ$, 3° step)
 - Single axis/dual axis
- Camera setup
 - Counting mode (ideally CDS mode on K3)
 - Short exposure times (per tilt dose $2-3 \text{ e}^-/\text{A}^2 \Rightarrow$ on K3 $\sim 0.5 \text{ sec}$)
 - Fractionation into few dose fractions (~ 4 fractions; $< 1 \text{ e}^-/\text{A}^2/\text{fraction}$)
- Energy filter setup
 - High-tilts \Rightarrow thick sample (more inelastically scattered electrons)
 - Zero loss mode – slit set to 10-20 eV
 - Increased contrast
- Phase-plate setup
 - Low dose low contrast \Rightarrow compensated by high defocus
 - Volta phase plate – comparable contrast at lower defocus (by applying phase shift on CTF)
- Combining SPA and tomography
 - Zero tilt acquired at higher dose ($10-20 \text{ e}^-/\text{A}^2$) – serves as micrograph for SPA
 - Other tilts acquired at standard dose

Energy filter, Volta phase plate (VPP)

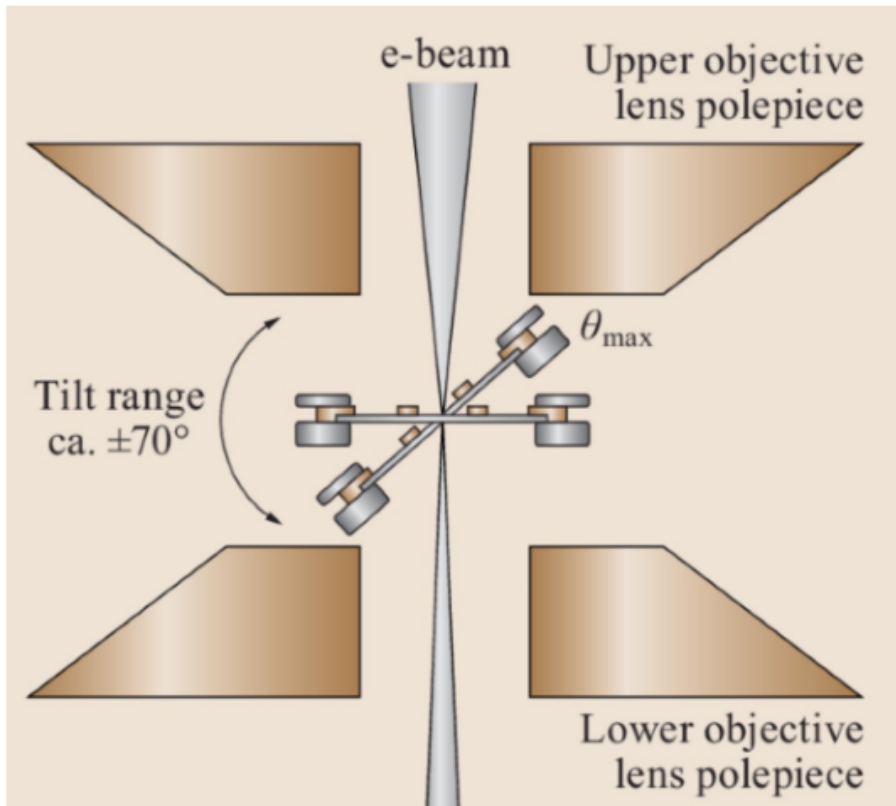


-5µm defocus, without VPP

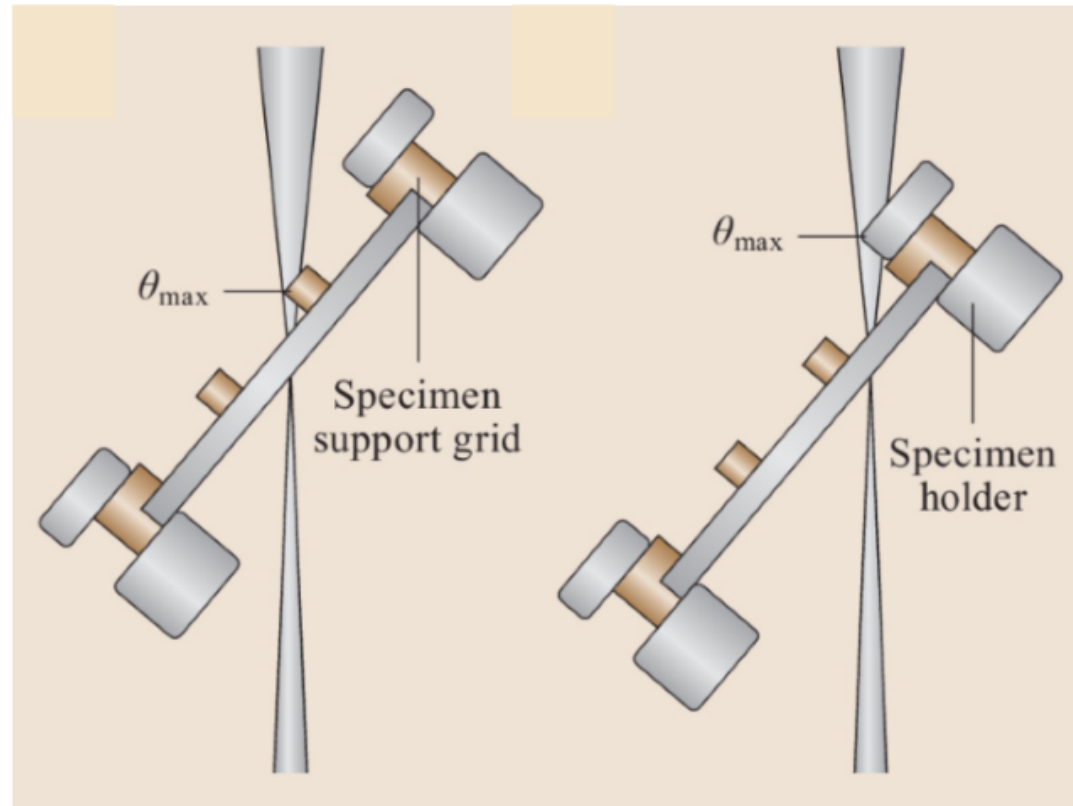


In focus, with VPP

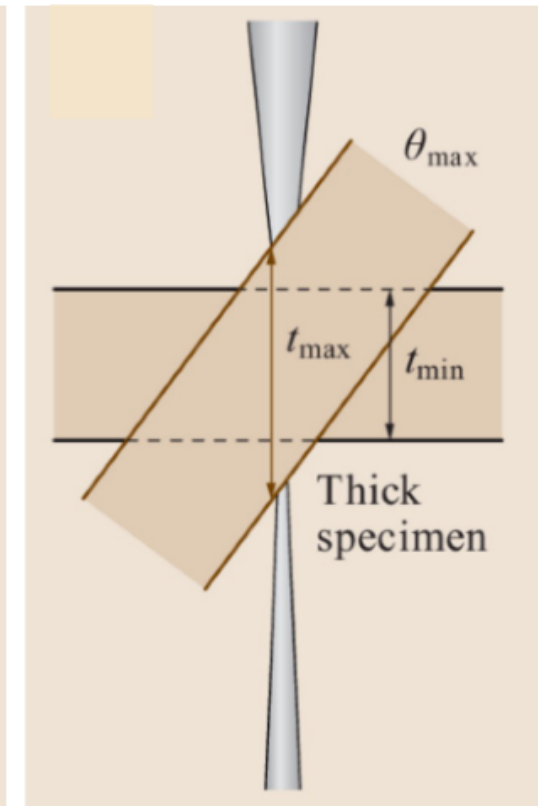
Tilt range limitation



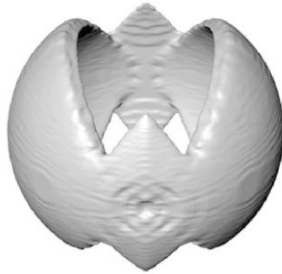
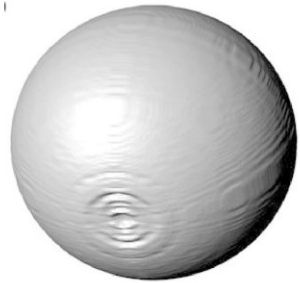
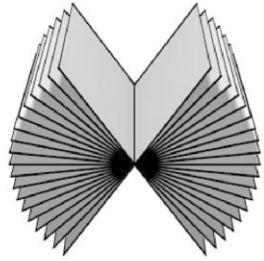
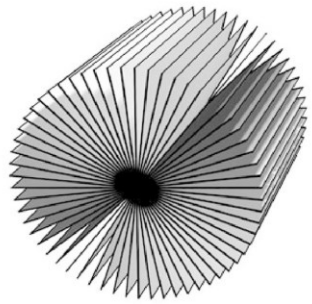
High tilt polepieces



Tomography holders



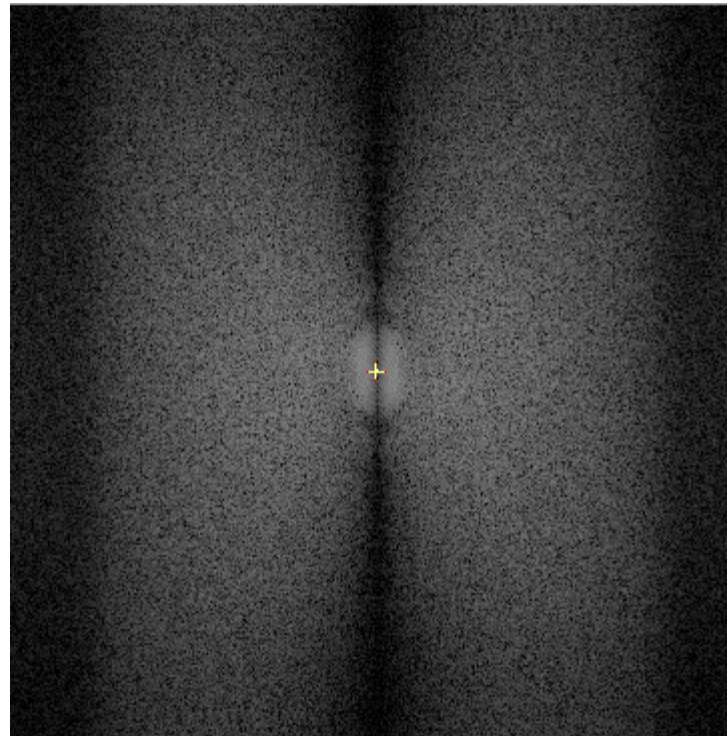
Missing wedge



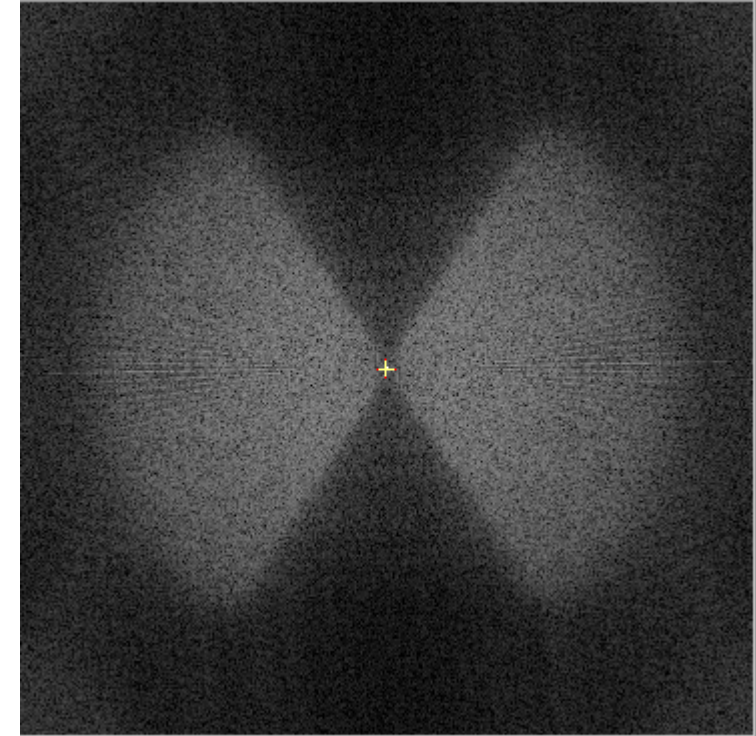
Ideal ($\pm 90^\circ$)

Real ($\pm 60^\circ$)

- Missing wedge – missing in Fourier space (therefore affects all the point in real-space)
- The information is missing there is no possibility to add it or recover it (it was not recorded at all)



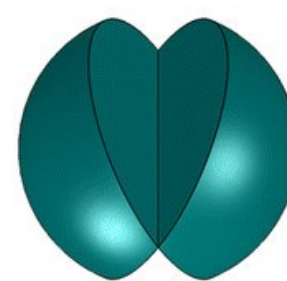
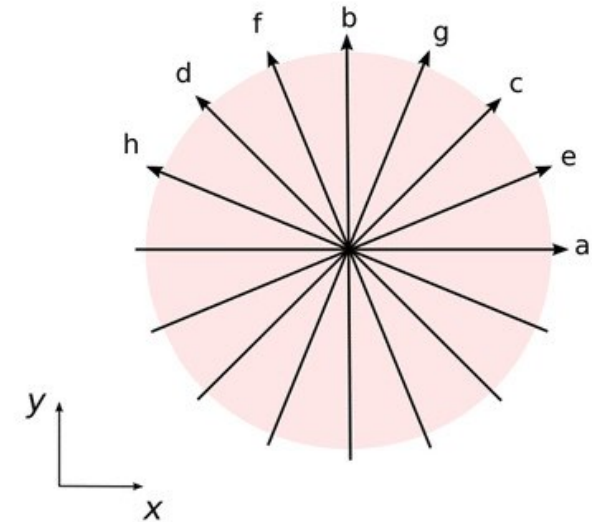
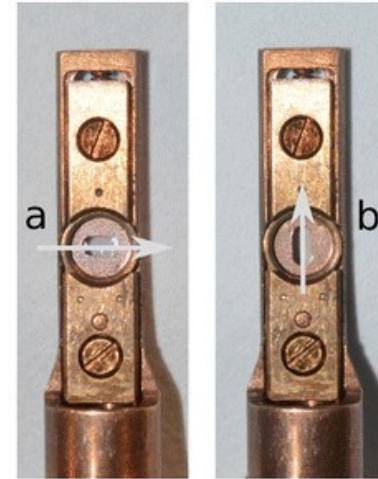
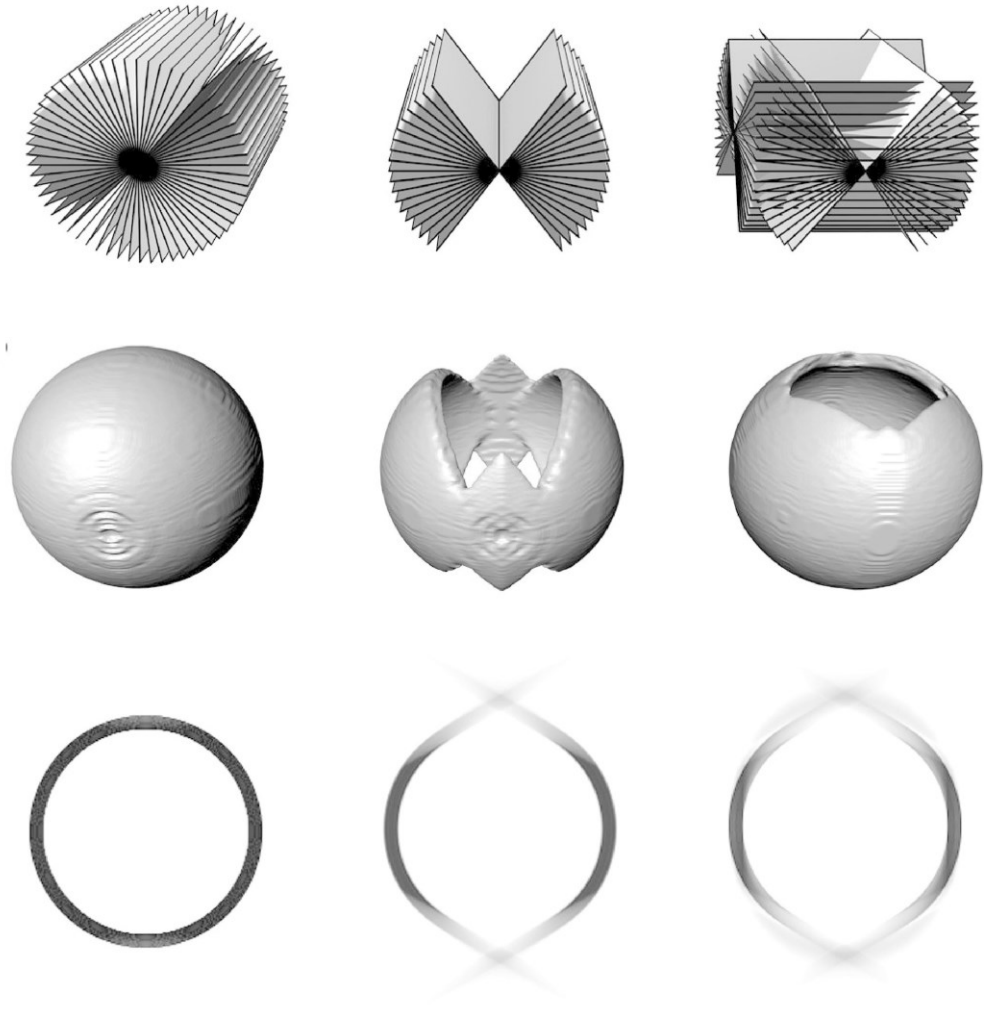
FFT XY plane of a tomogram slice



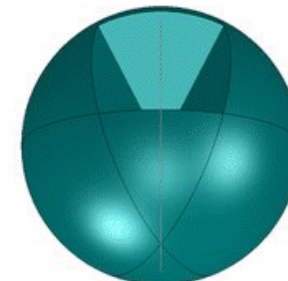
FFT XZ plane of a tomogram slice

Dual (multi) tilt tomography

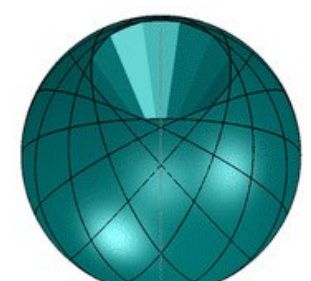
- Dual-axis sample holders



Single Tilt



Double Tilt



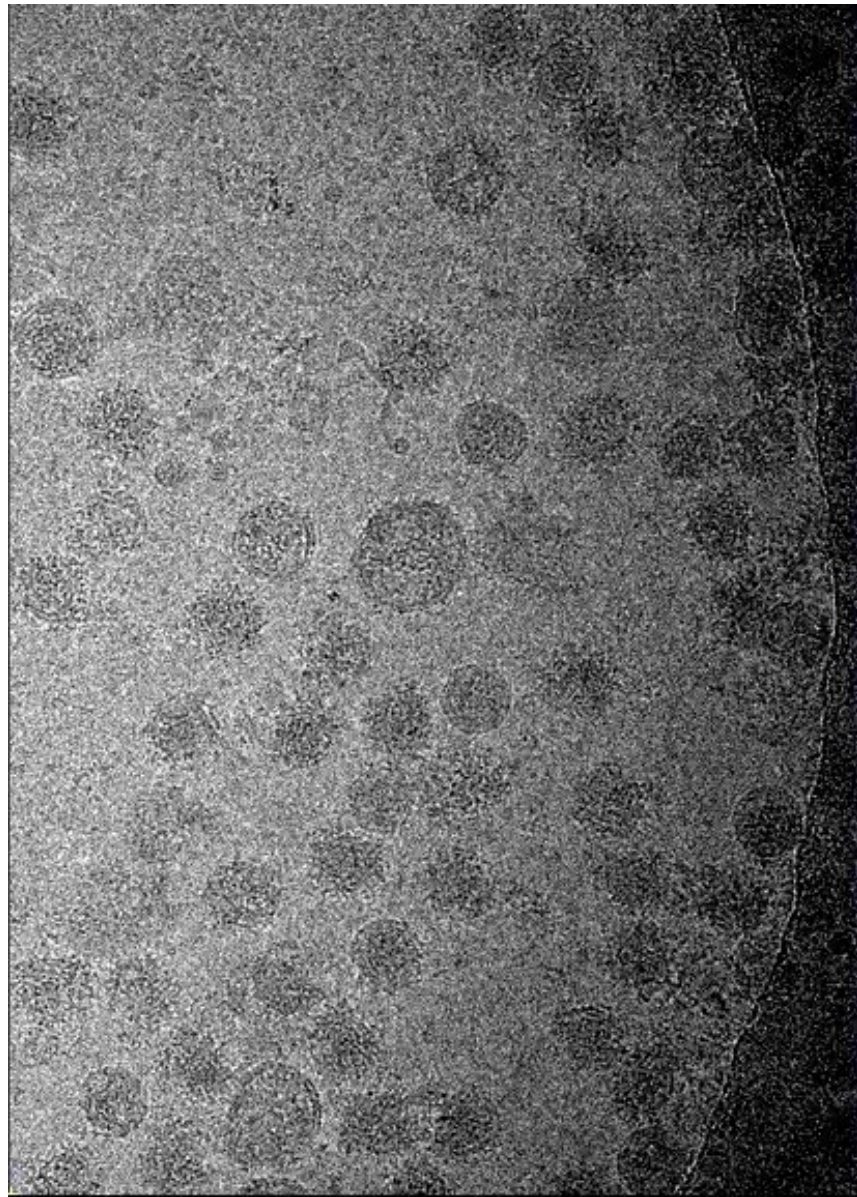
Eight-Tilt

Tomography - Data processing

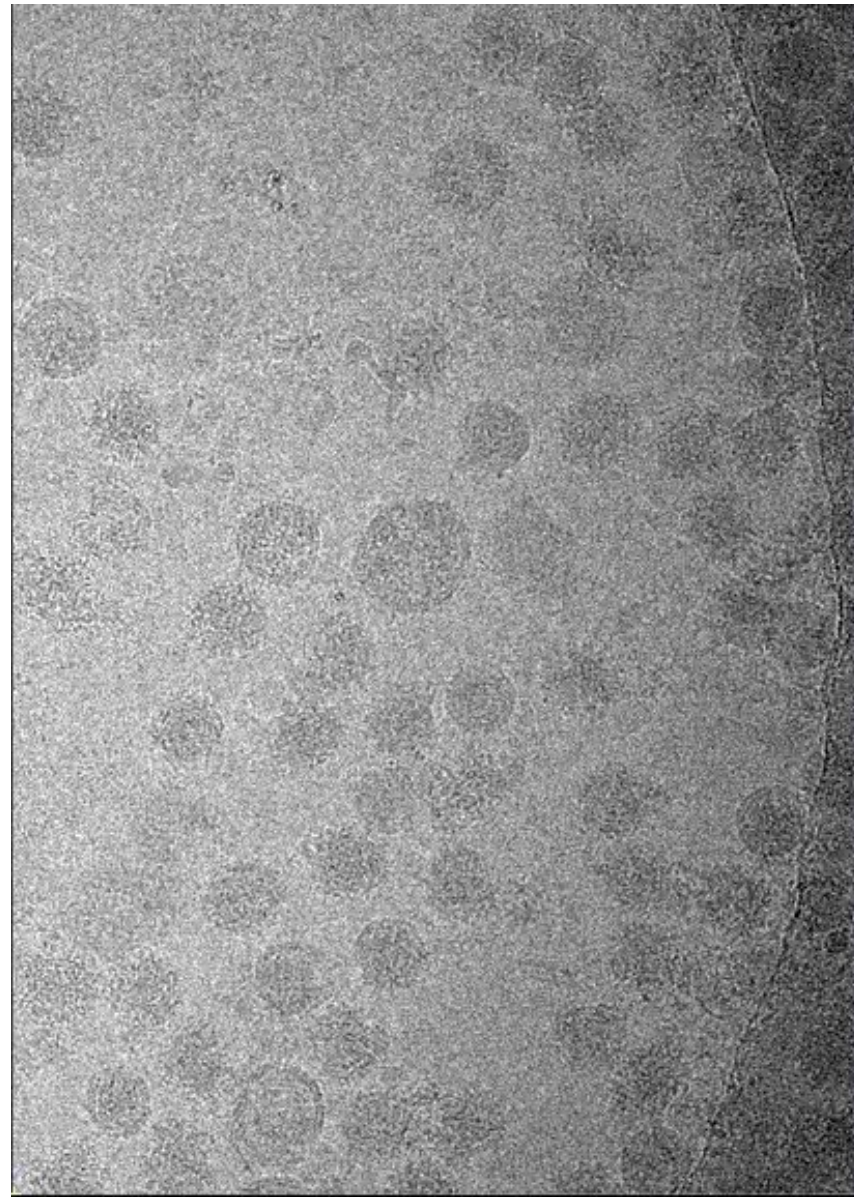
- Motion correction of raw movie data of single tilts
 - Possibility of dose weighting of single tilts
- Alignment of tilt series
 - Coarse alignment – cross correlation between neighboring tilts
 - Fine alignment – fiducial model that describe the tilting transformations
- Aligned tilt series postprocessing
 - Fiducial removal, CTF correction
- Reconstruction of the tomogram
 - Back-projection algorithms
- Tomogram filtering
- Segmentation of tomogram
- Sub-tomogram averaging
 - Refining a high-resolution structure from the subparts of the tomogram

Tilt alignment – Coarse align

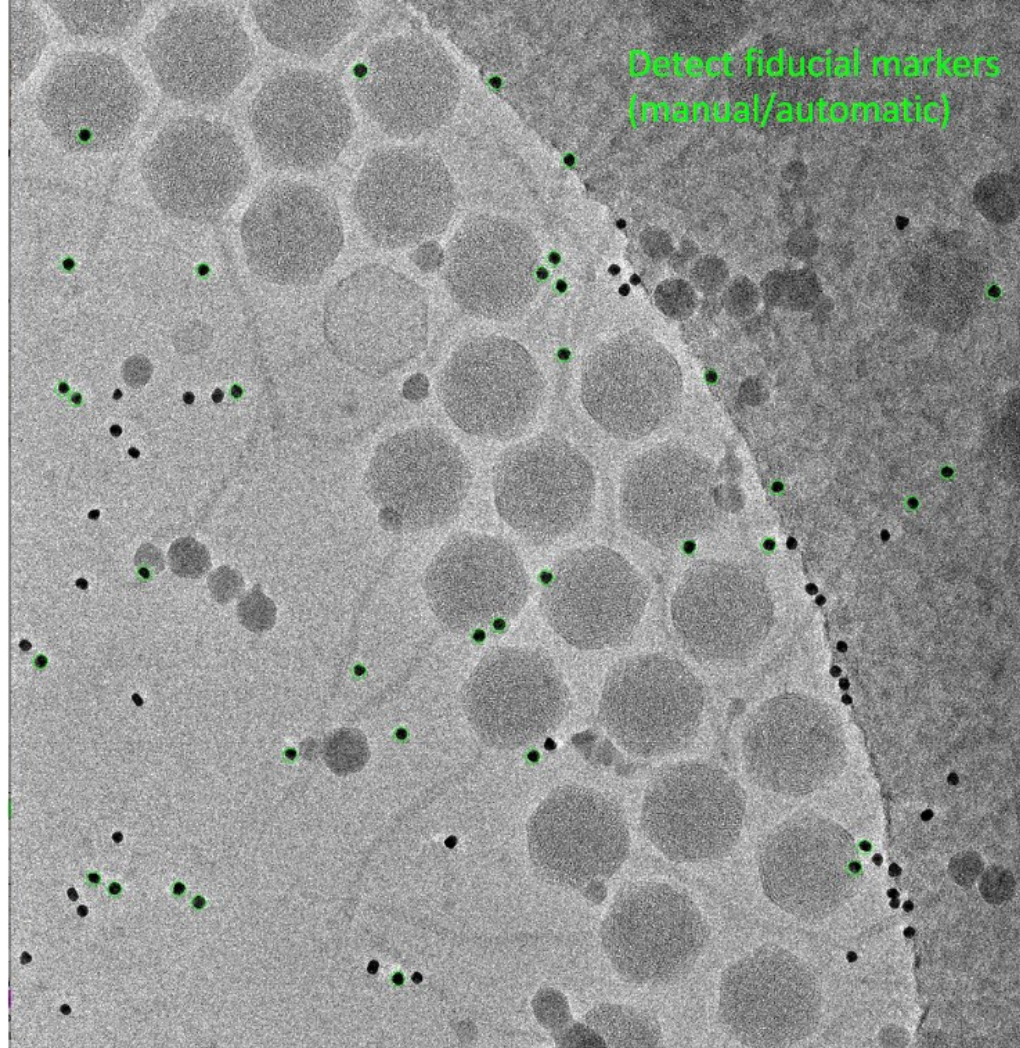
After acquisition



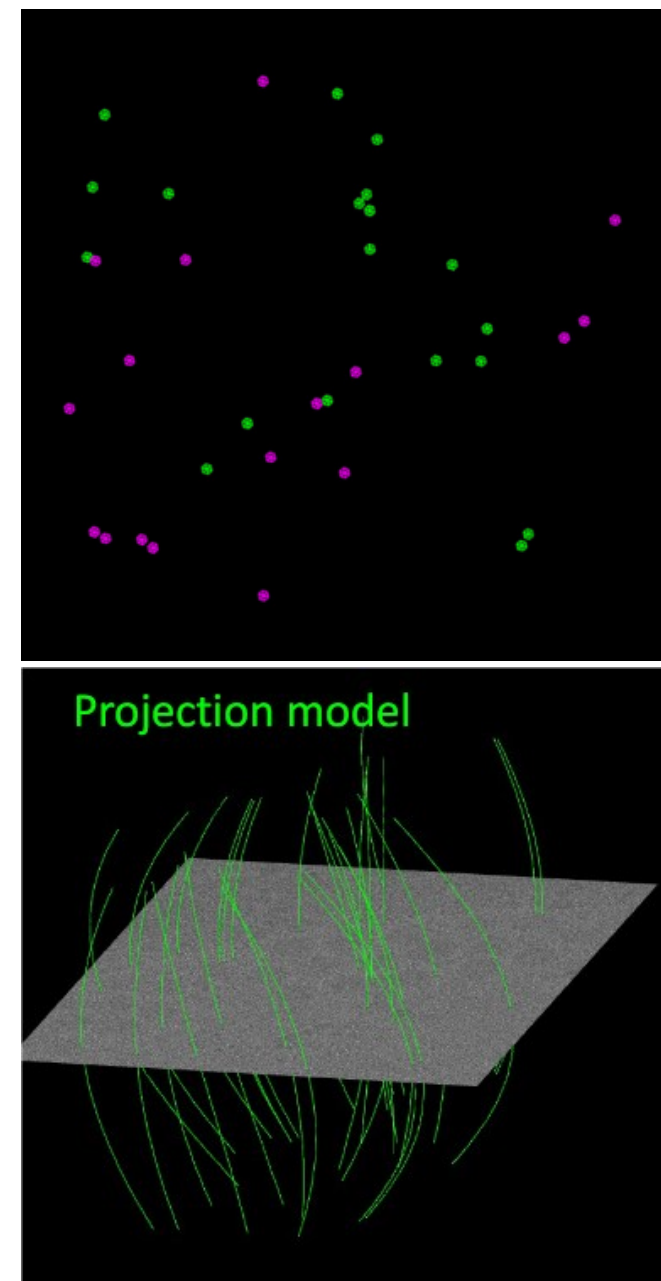
After coarse alignment



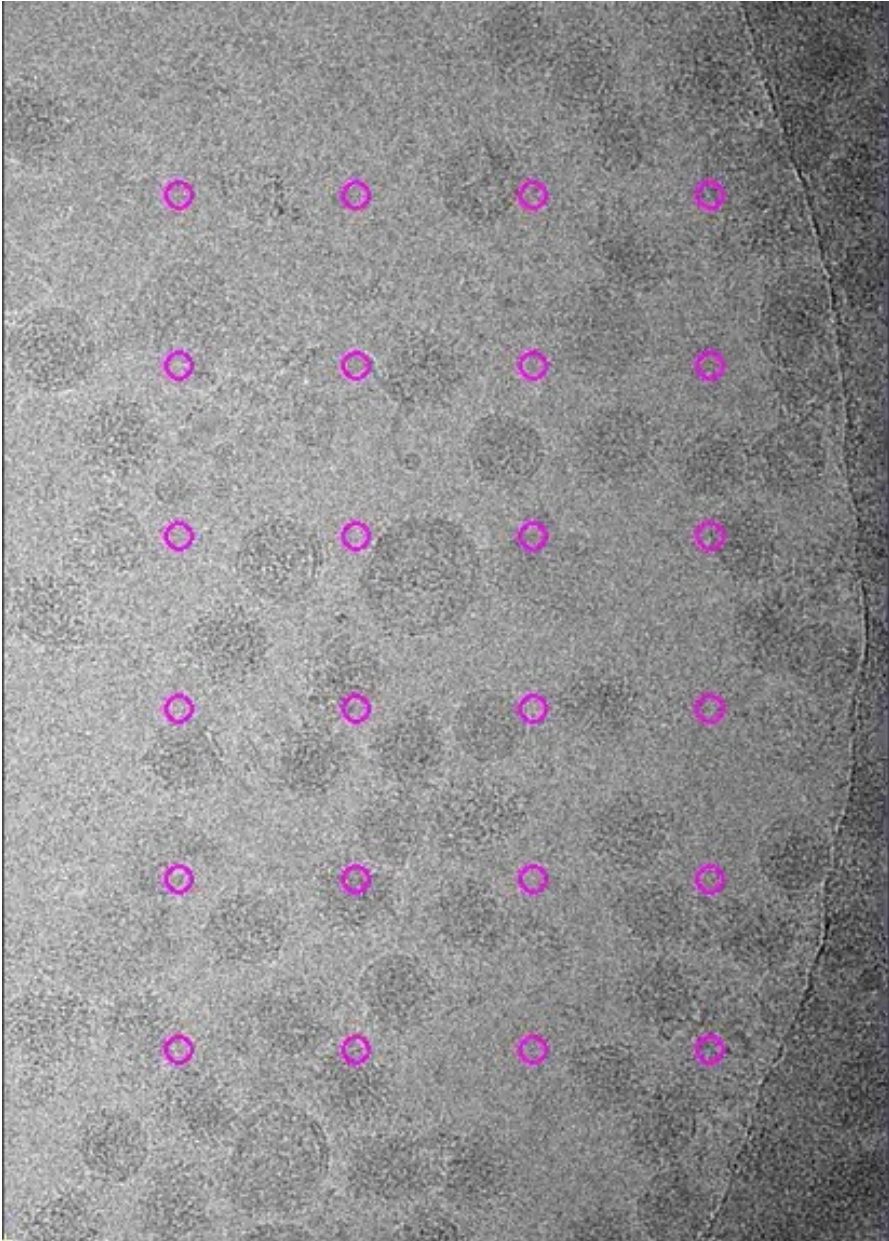
Fiducial based fine alignment



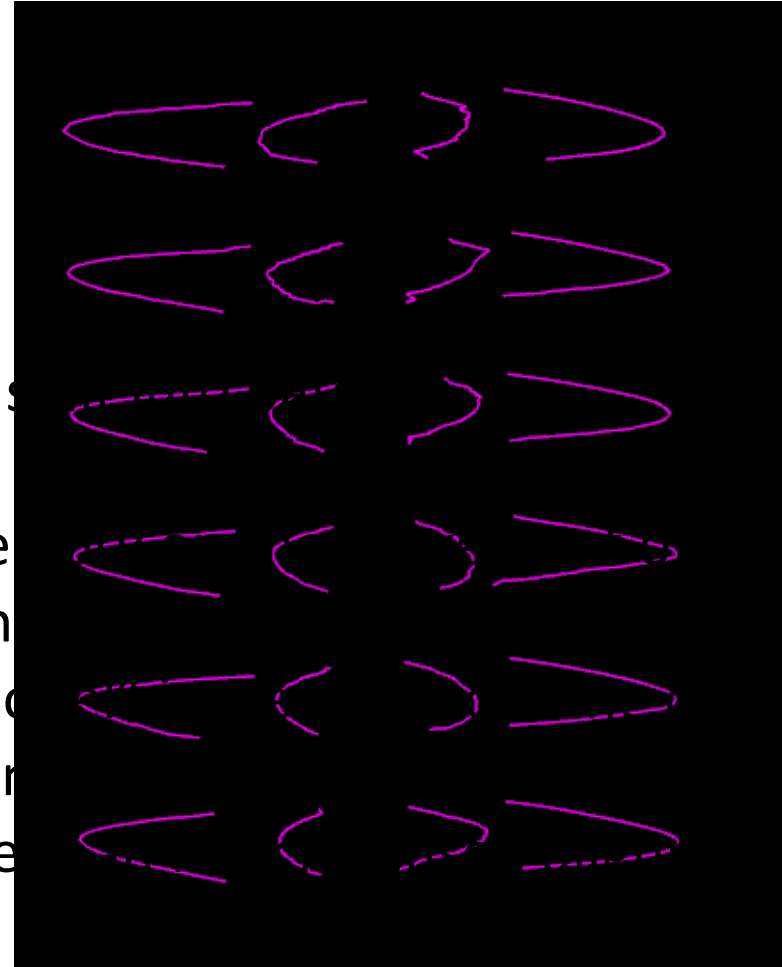
- Need fiducials
- Finding the same fiducial on all of the tilts and fitting a model on their trajectory
- Allows subpixel precision alignment of tilt series



Patch tracking – fine alignment



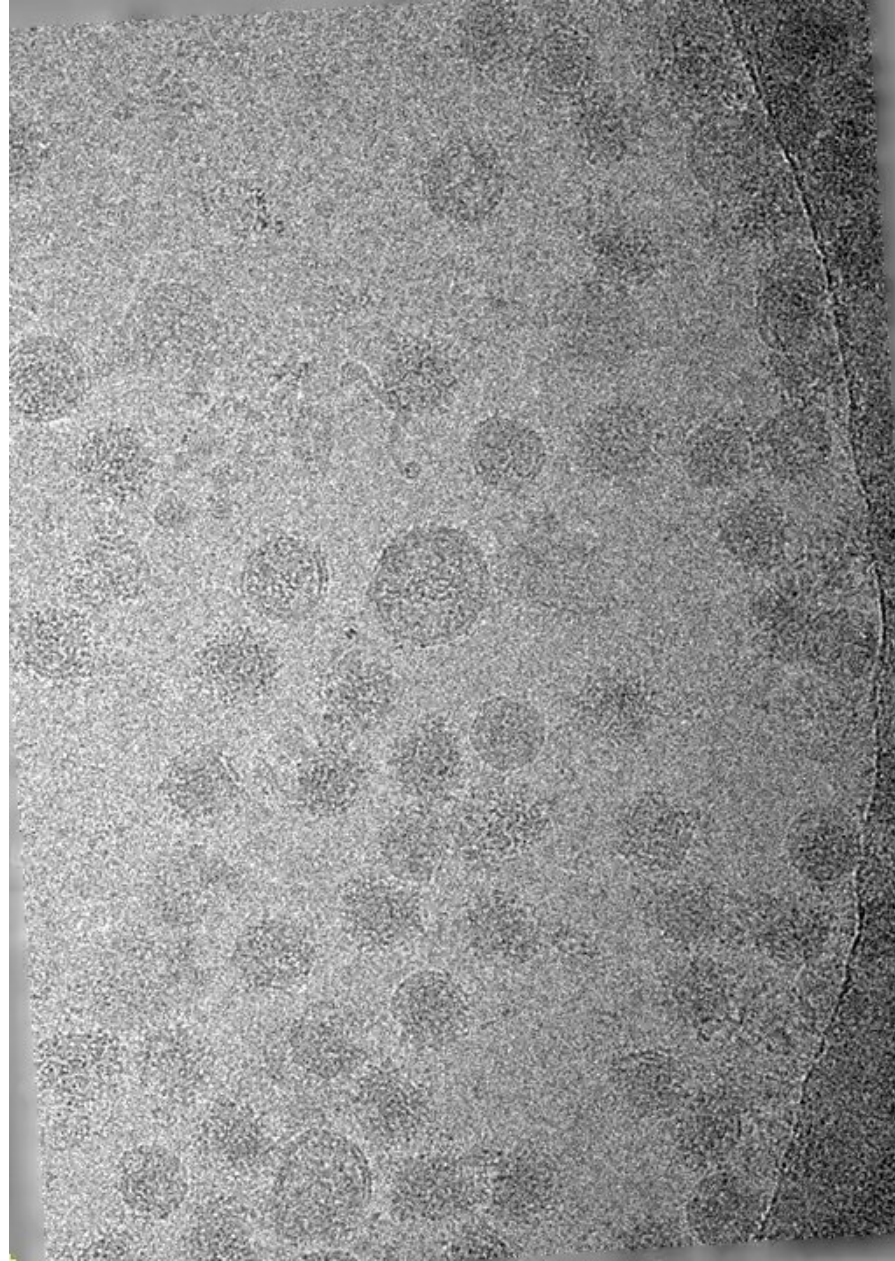
- Tilt images s
- Correlating
- Fitting traje
- Every patch
- “Fiducial mo
- any addition
- Less precise



patches
be traceable
itself without
t models

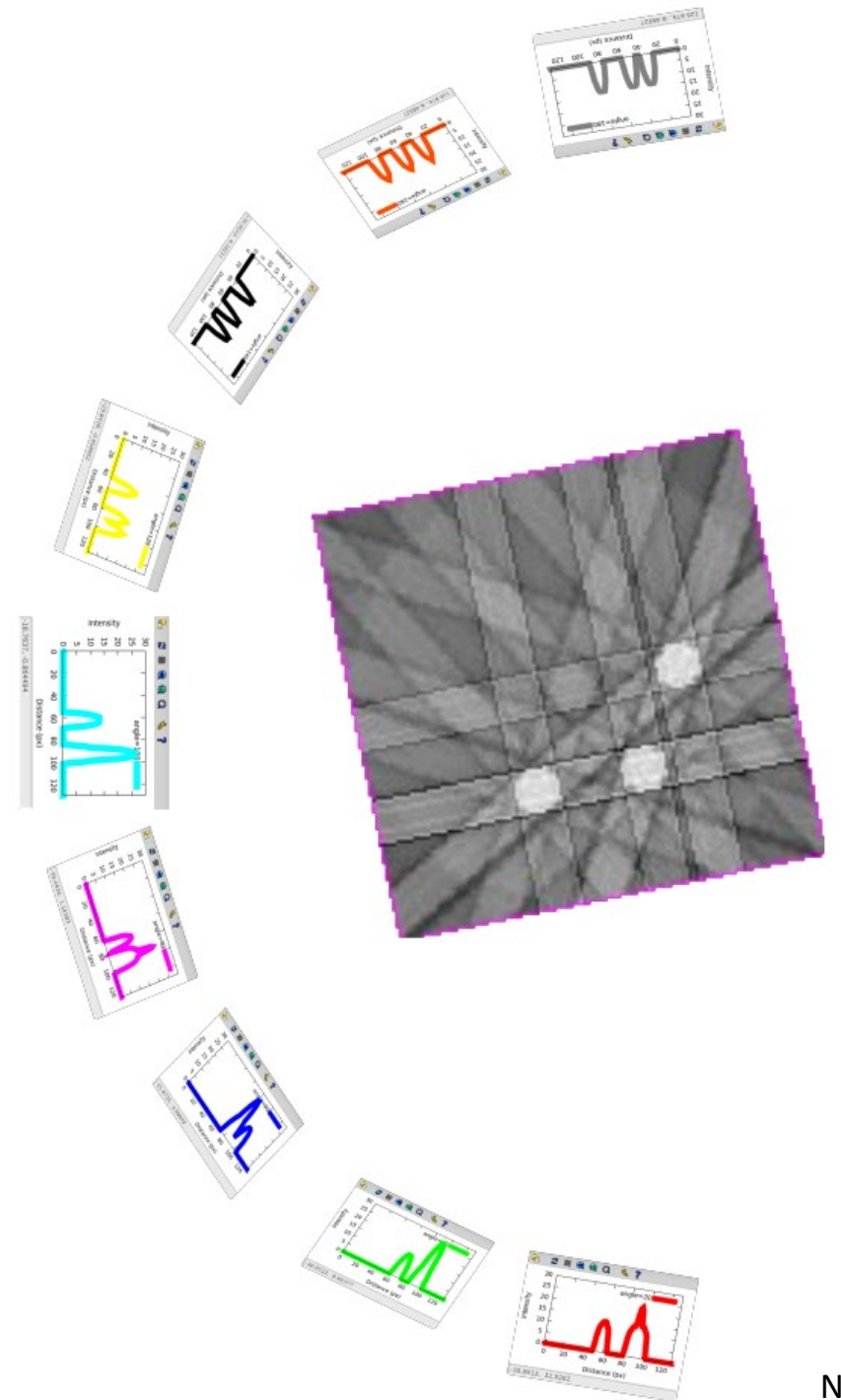
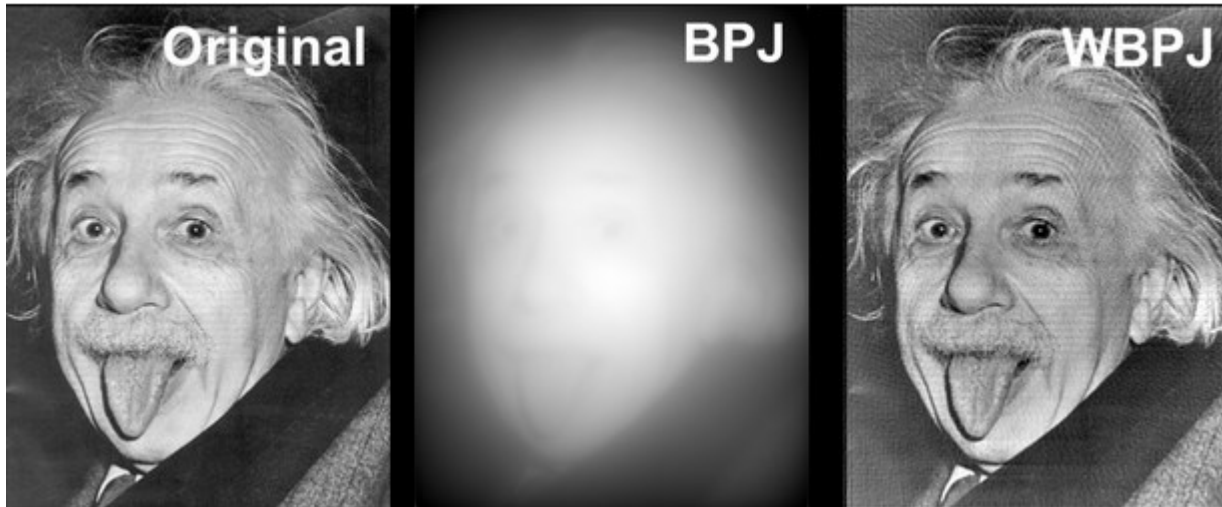


Fine alignment using the fiducial model



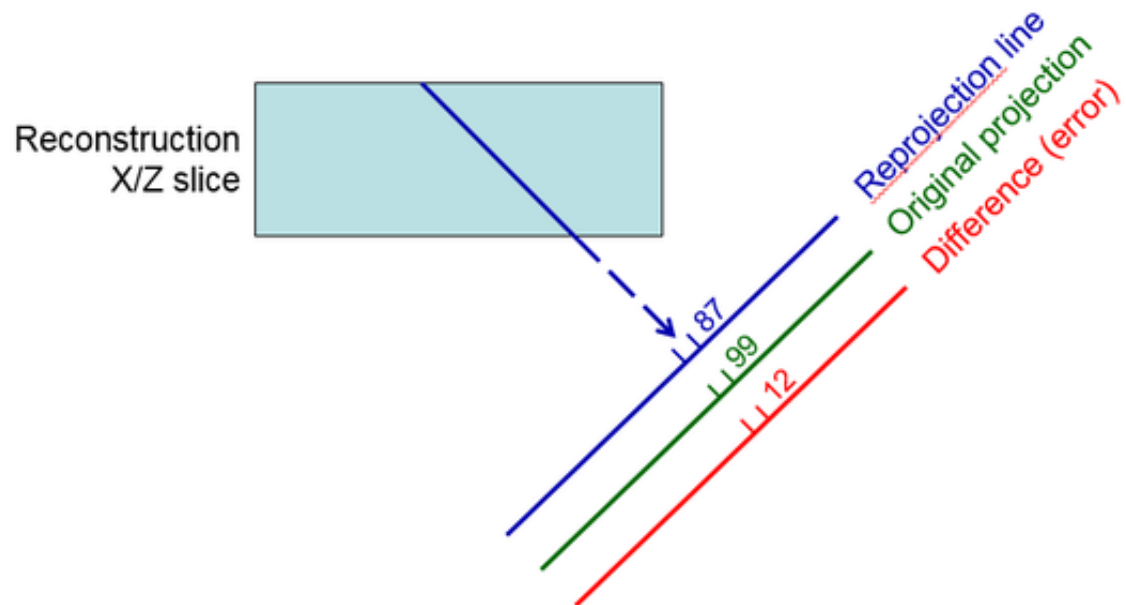
Reconstruction

- Back-projection
 - Low frequencies are over-represented
- Weighted back-projection
 - Low frequencies are down weighted
- SIRT
 - Simultaneous Iterative Reconstruction Technique



SIRT (Simultaneous Iterative Reconstruction Technique)

- Start with a tomogram reconstruction from the backprojection of the tilts
- Reprojecting from the tomogram in the original tilt orientations
- Taking the difference between the original projection data and this reprojection at each pixel (this difference represents the amount of error in the current estimate)
- Adding the error to the tomogram by a back-projection operation

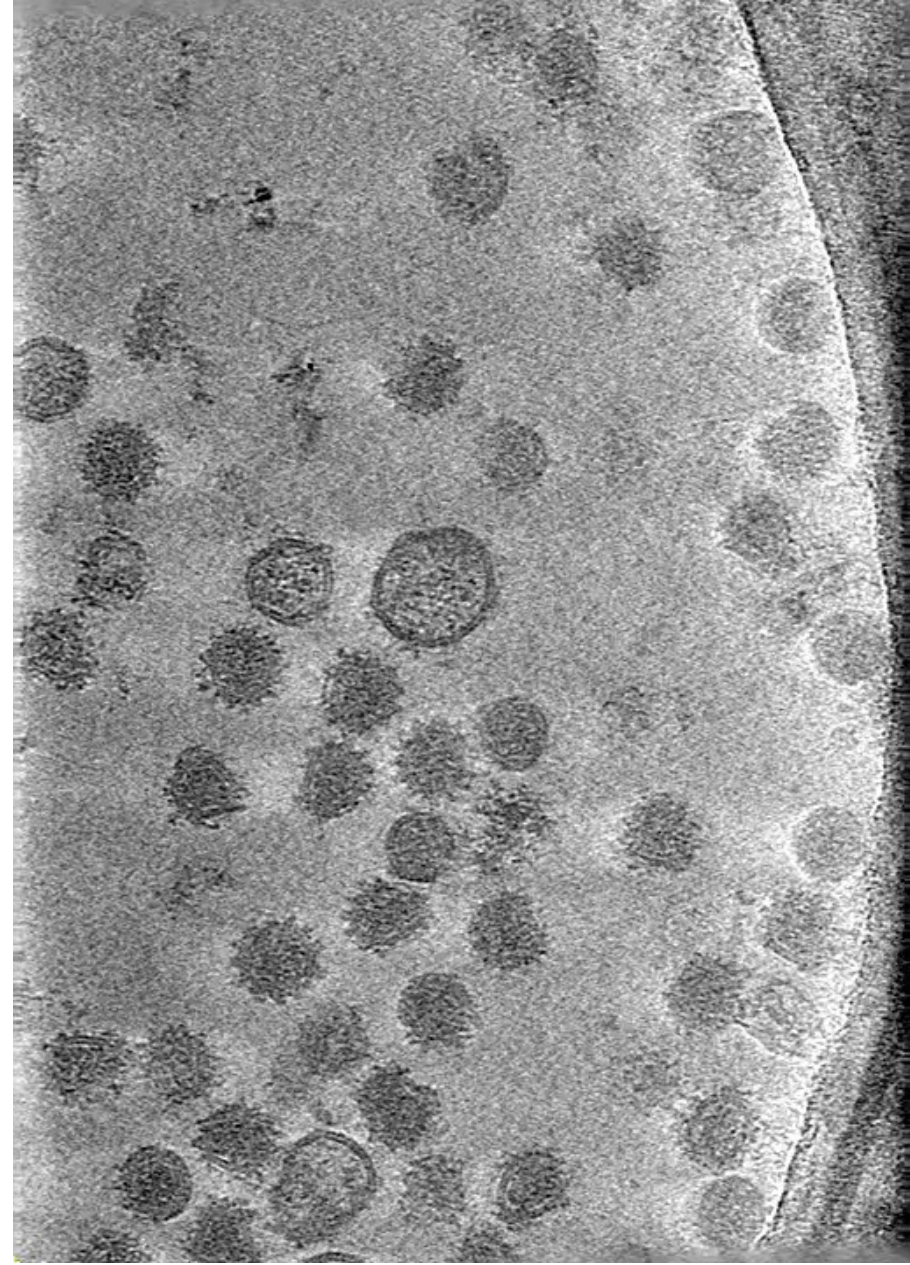


Reconstruction

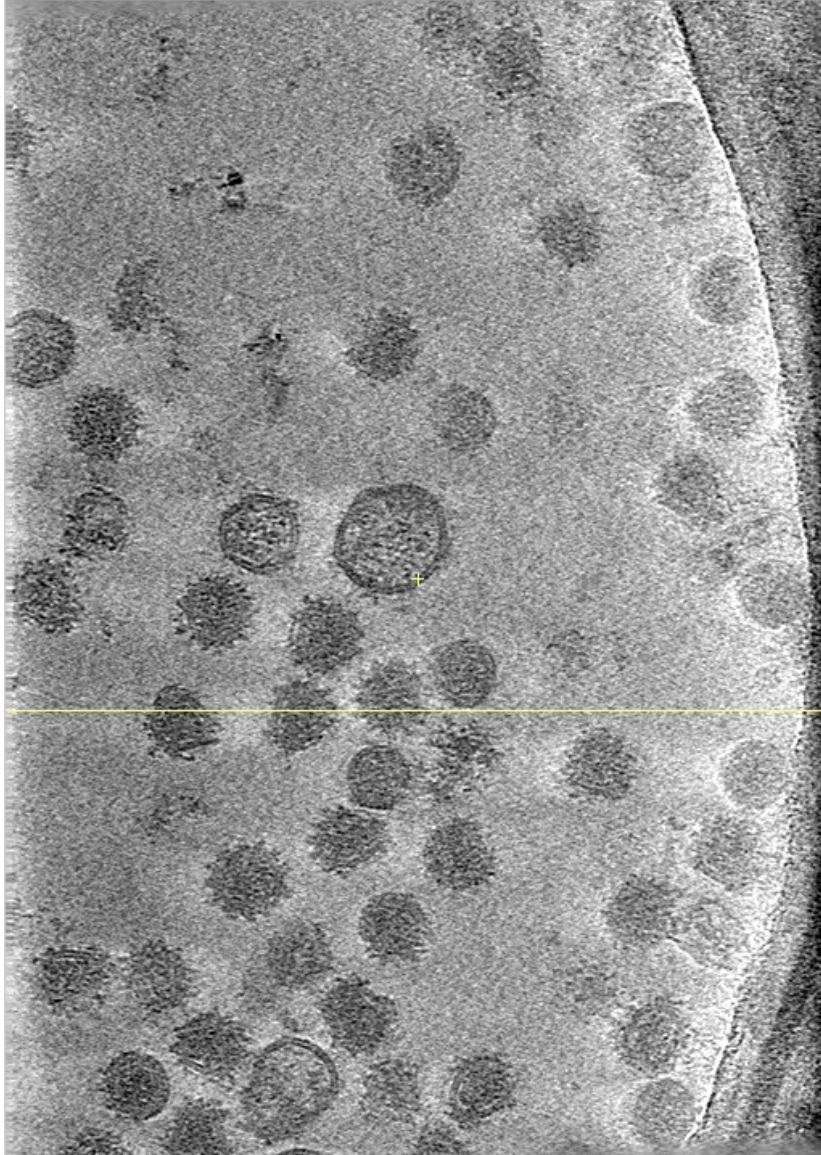
**Weighted
Back-projection**



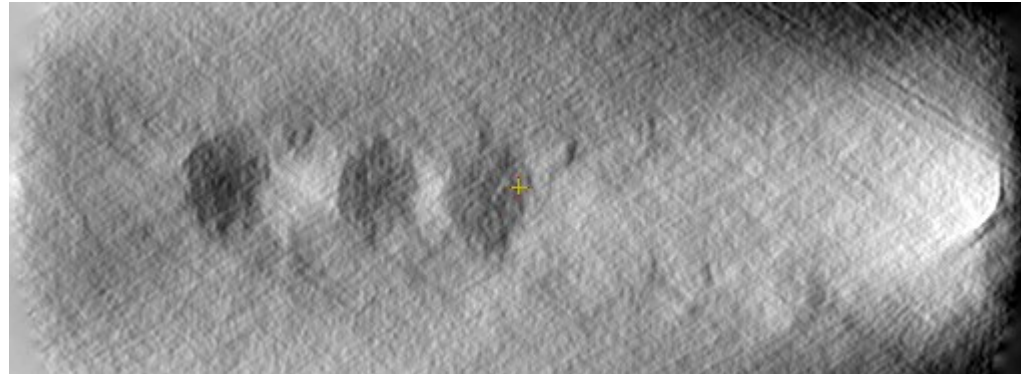
SIRT



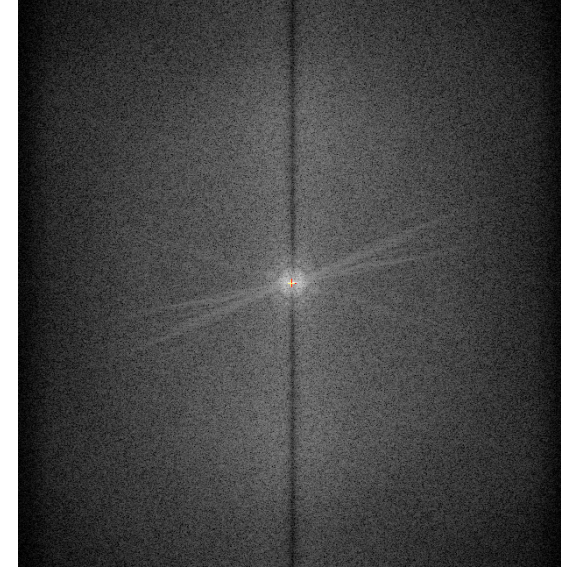
Missing wedge



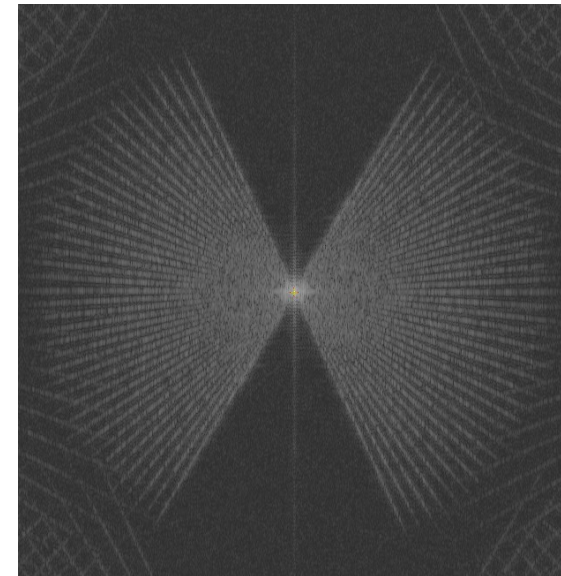
XY Plane



XZ Plane



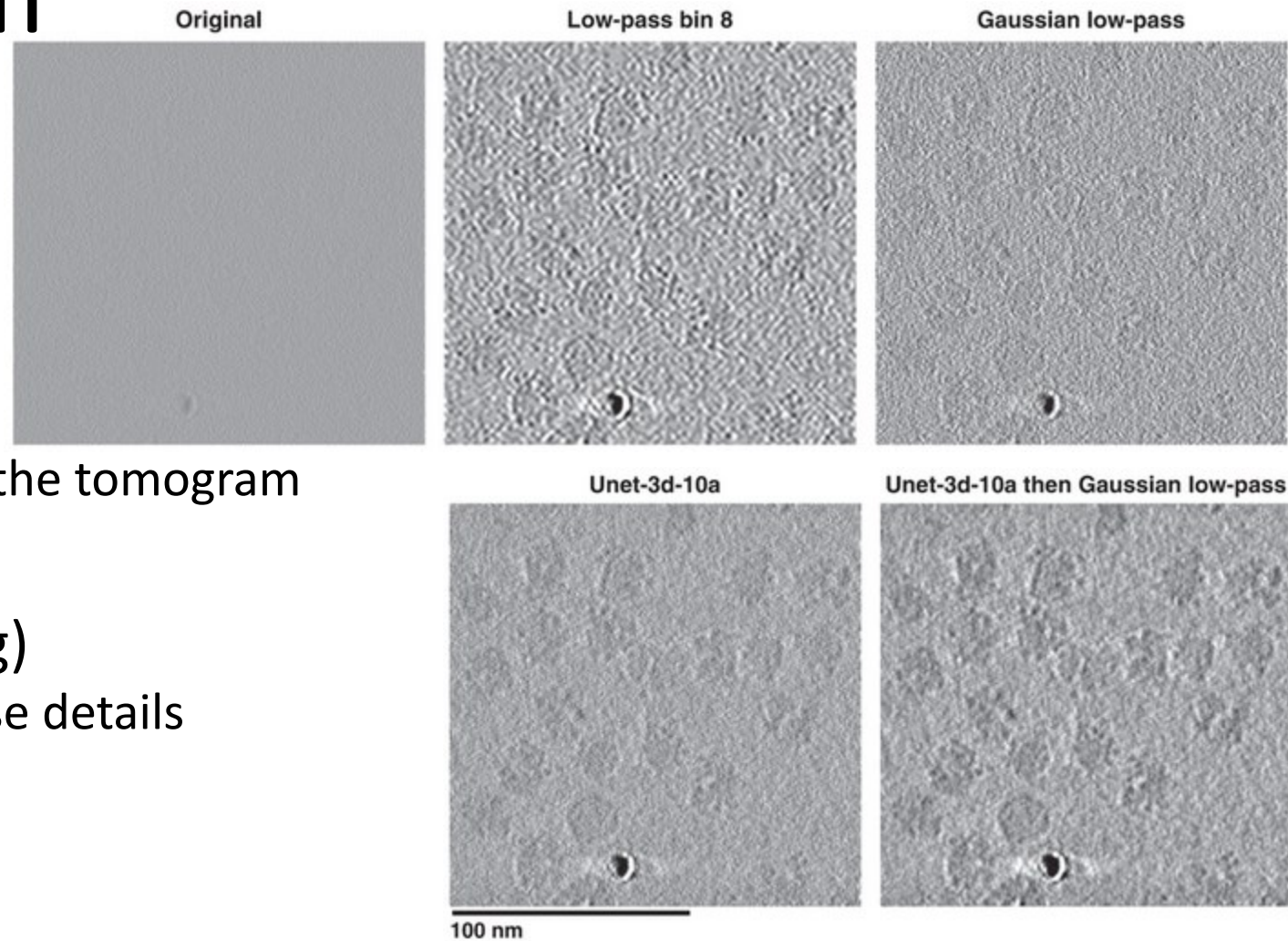
FFT XY Plane



FFT XZ Plane

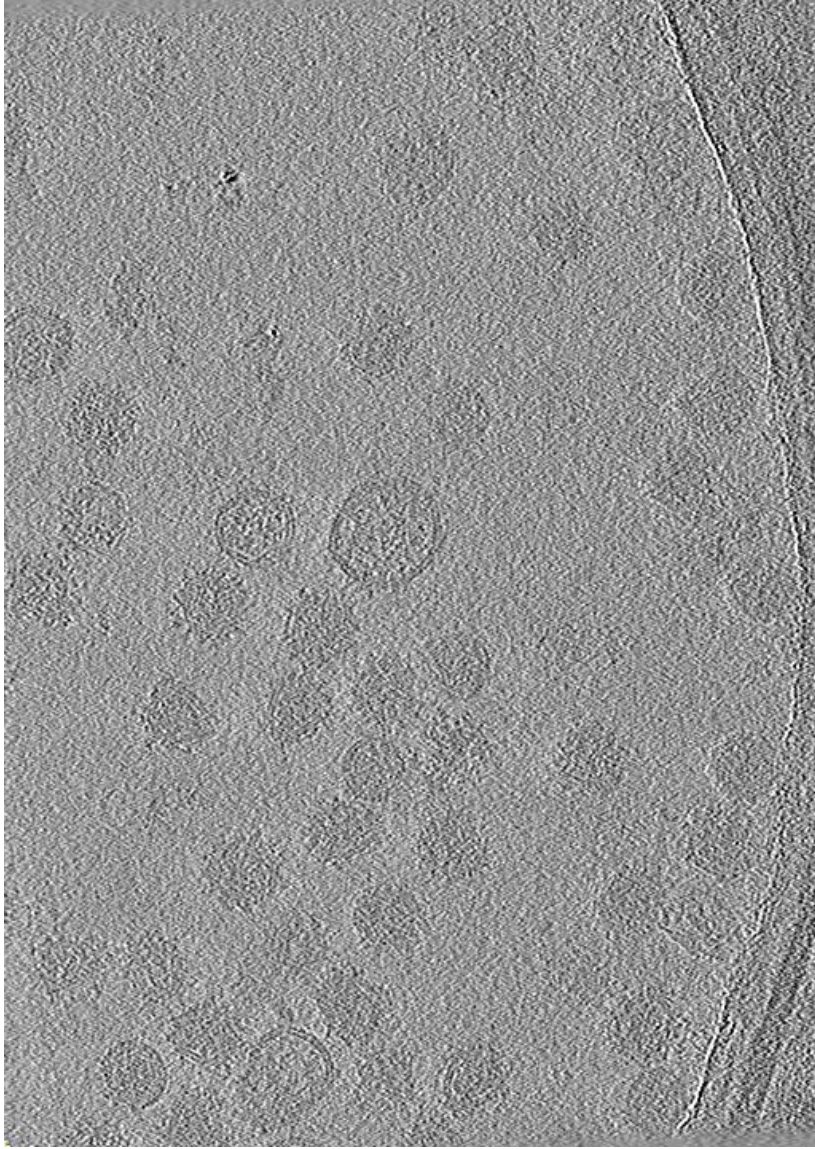
Tomogram interpretation

- Visual inspection
 - Annotation of features
- Segmentation
 - Annotating/extracting segments from the tomogram
- Sub-tomogram averaging
- Filtering – postprocessing (denoising)
 - Lowpass filters – increase contrast loose details
 - High pass filters – edge detection
 - Median filters
 - NAD – Nonlinear Anisotropic diffusion
 - Need to be tuned for balance between contrast and preserved details
 - Neural network based denoising
 - Noise model trained on data

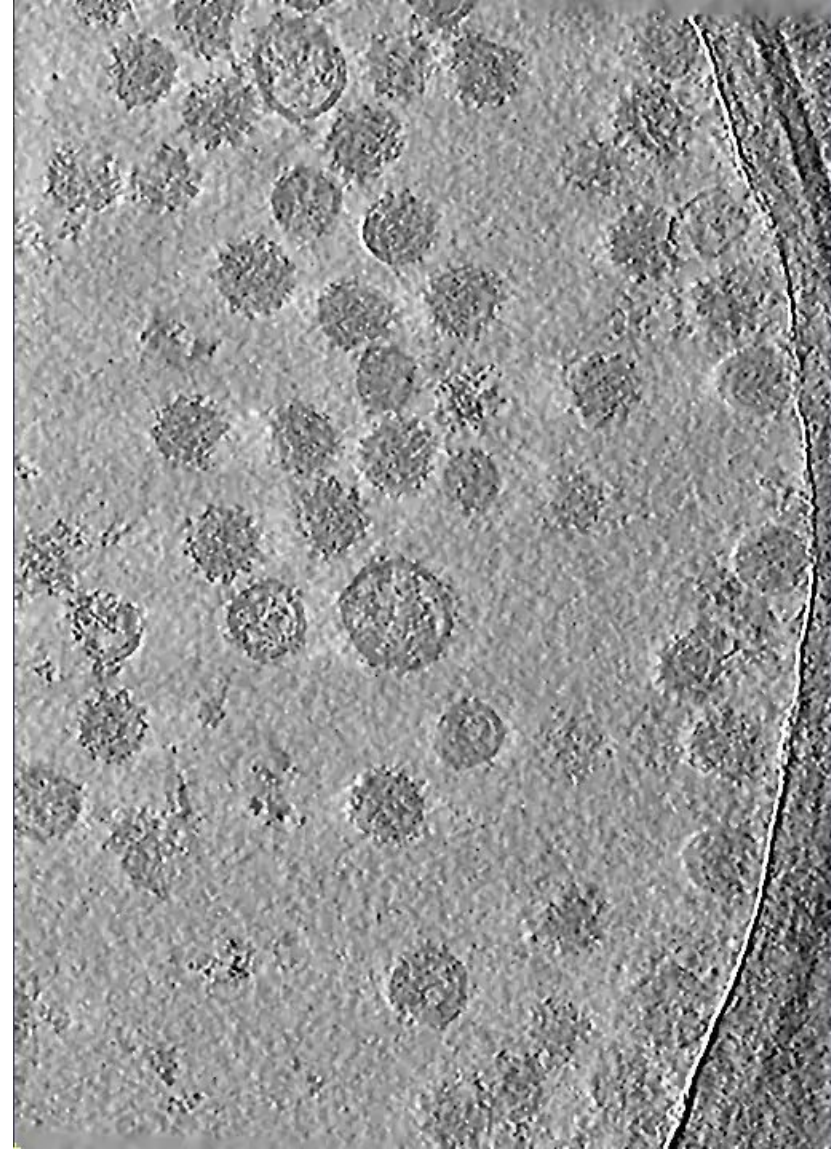


NAD – nonlinear anisotropic diffusion

Before



After

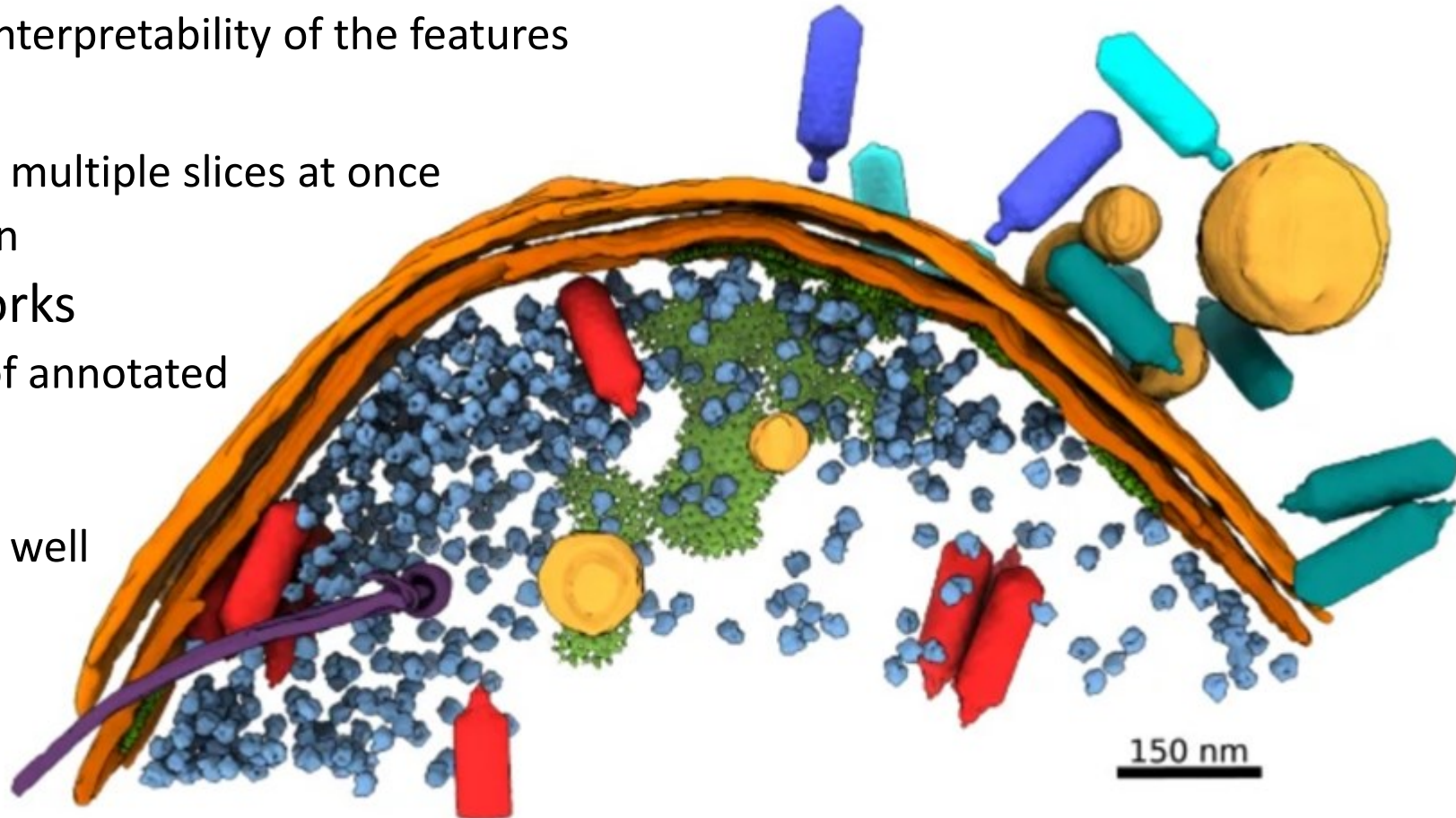


Segmentation

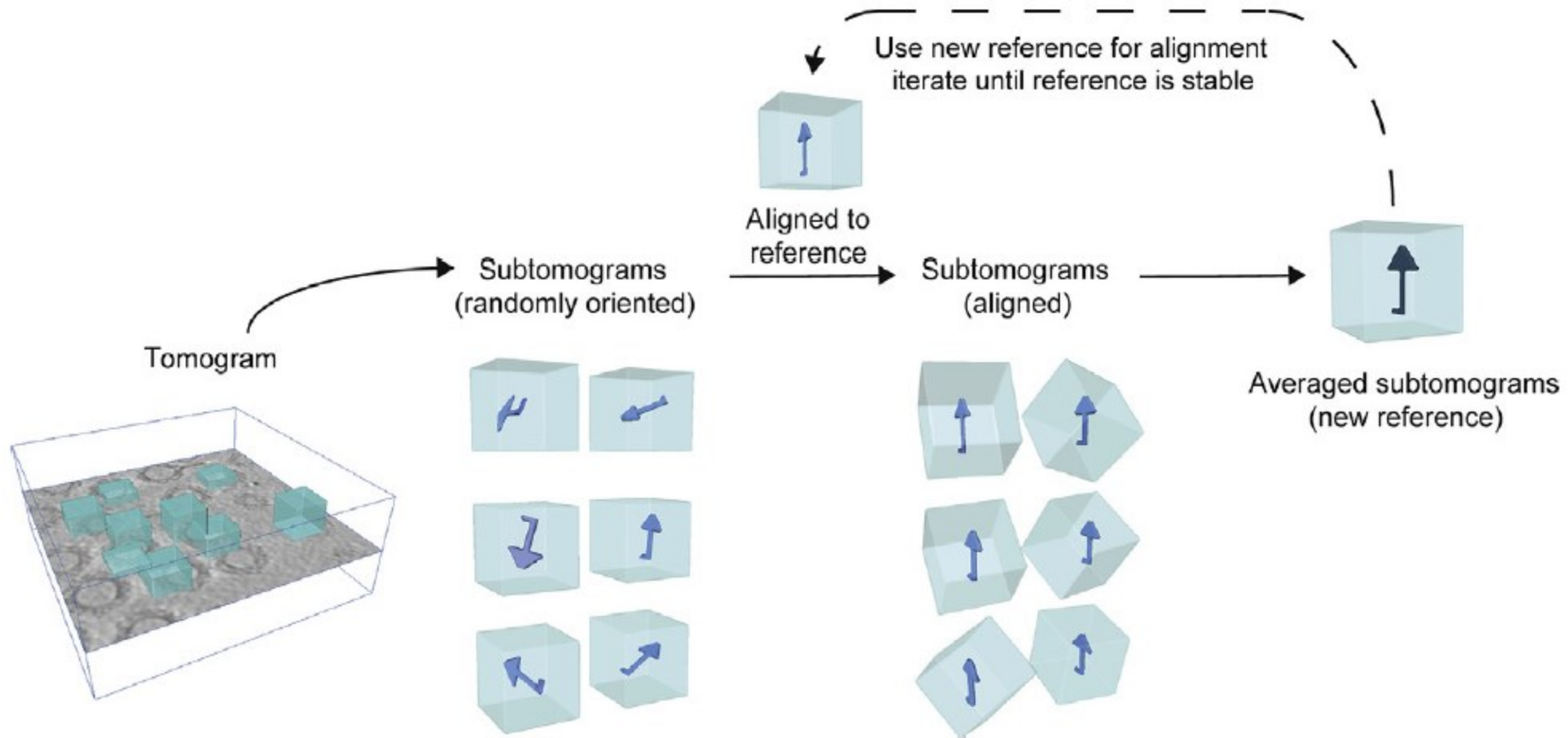


Segmentation

- Annotating parts of the tomogram by connecting continuous segments
 - Manual
 - Drawing
 - Thresholding
 - “Missing wedge” limits the interpretability of the features
 - Semiautomatic
 - Simultaneous annotation on multiple slices at once
 - Correlation based annotation
 - Convolutional neural networks
 - Training CNN on small part of annotated tomogram
 - Long training process
 - General models not working well



Sub-tomogram averaging



- Increasing signal to noise ratio
- Increasing resolution
- By averaging uniformly orientationally distributed sub-tomograms we fill the missing wedge in the Fourier space

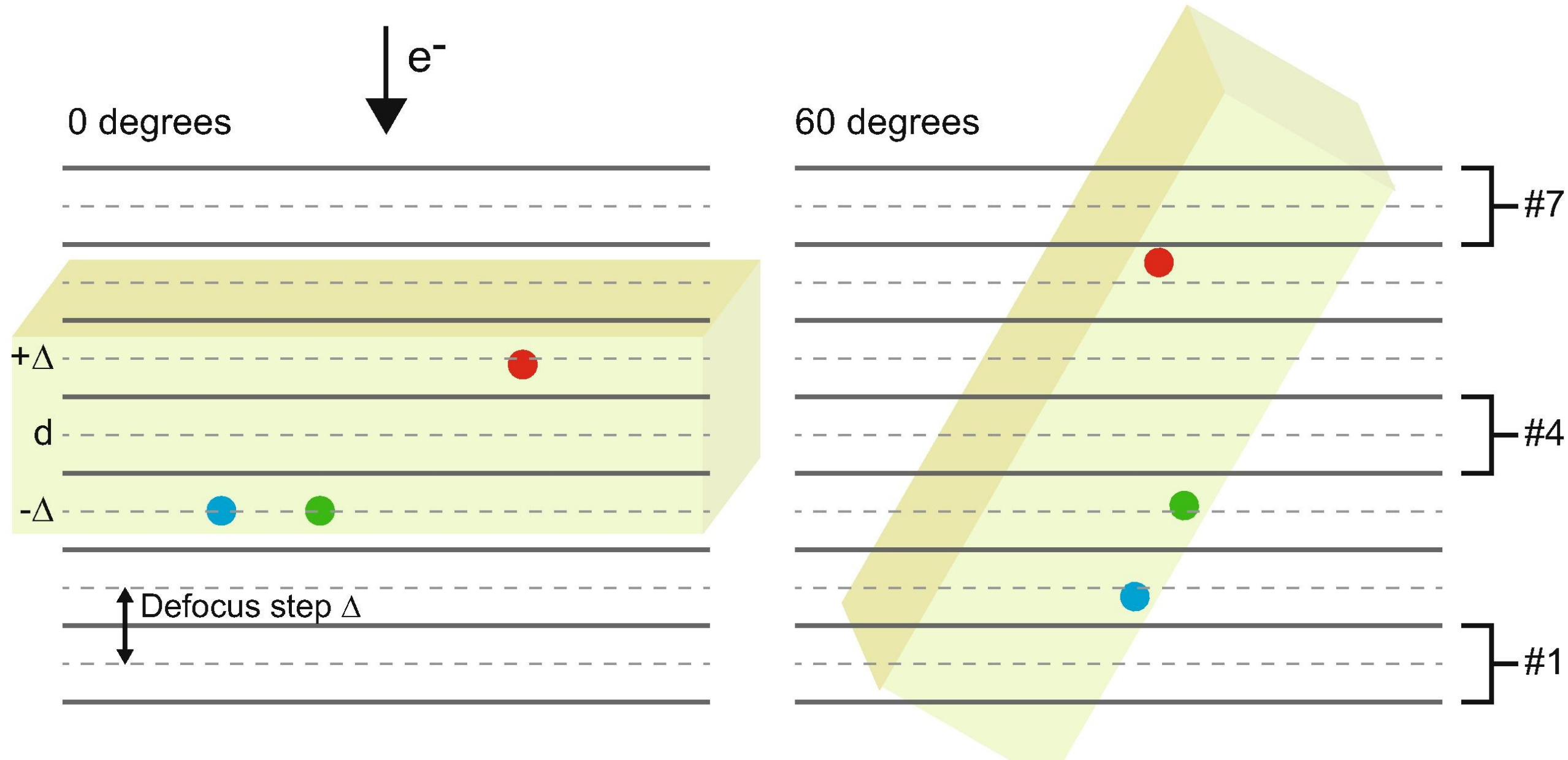
Tilt-dose weighting

- High angle tilts heavily radiation damaged
 - Not containing high resolution information
- Essential for high resolution sub-tomogram averaging
- Dose weighting during movie motion correction process
- Implemented in many sub-tomogram averaging software
 - Beware not to double dose weight the data

$$\begin{array}{c}
 \text{Spatial frequency} \\
 \uparrow \\
 q(k, N) = e^{-\frac{N}{2N_e(k)}} \\
 \downarrow \quad \downarrow \\
 \text{exposure-dependent} \quad \text{accumulated exposure} \\
 \text{amplitude attenuation} \quad \text{of the frame}
 \end{array}
 \qquad
 \begin{array}{c}
 \tilde{F}^W(\mathbf{k}) \\
 \downarrow \\
 \text{Dose-weighted} \\
 \text{Fourier transform of Image}
 \end{array}
 = \frac{\sum_{i=1}^n q(k, N_i) F_i(\mathbf{k})}{\sqrt{\sum_{i=1}^n q(k, N_i)^2}}$$

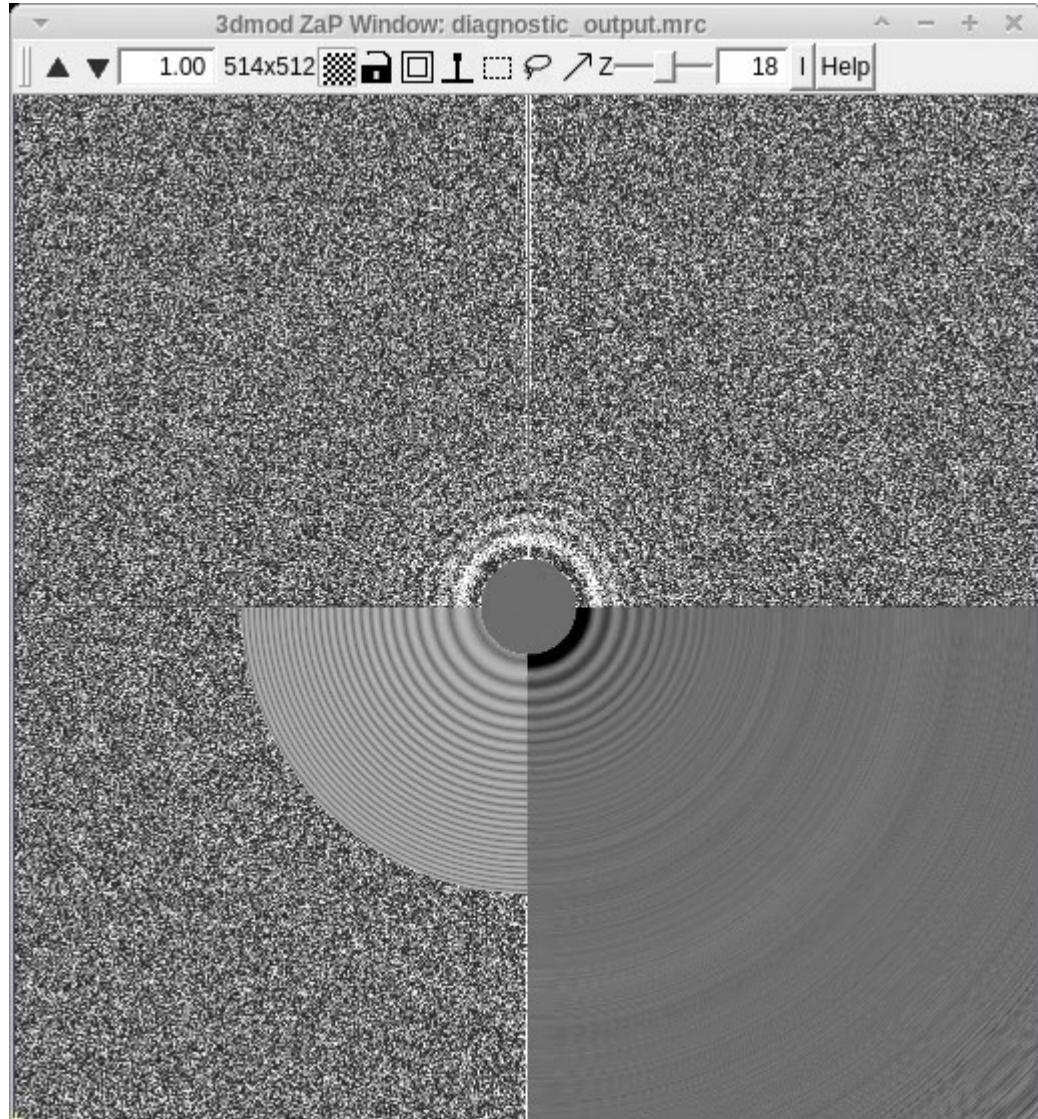
\downarrow
 i-th fraction / i-th tilt

CTF estimation – defocus gradient

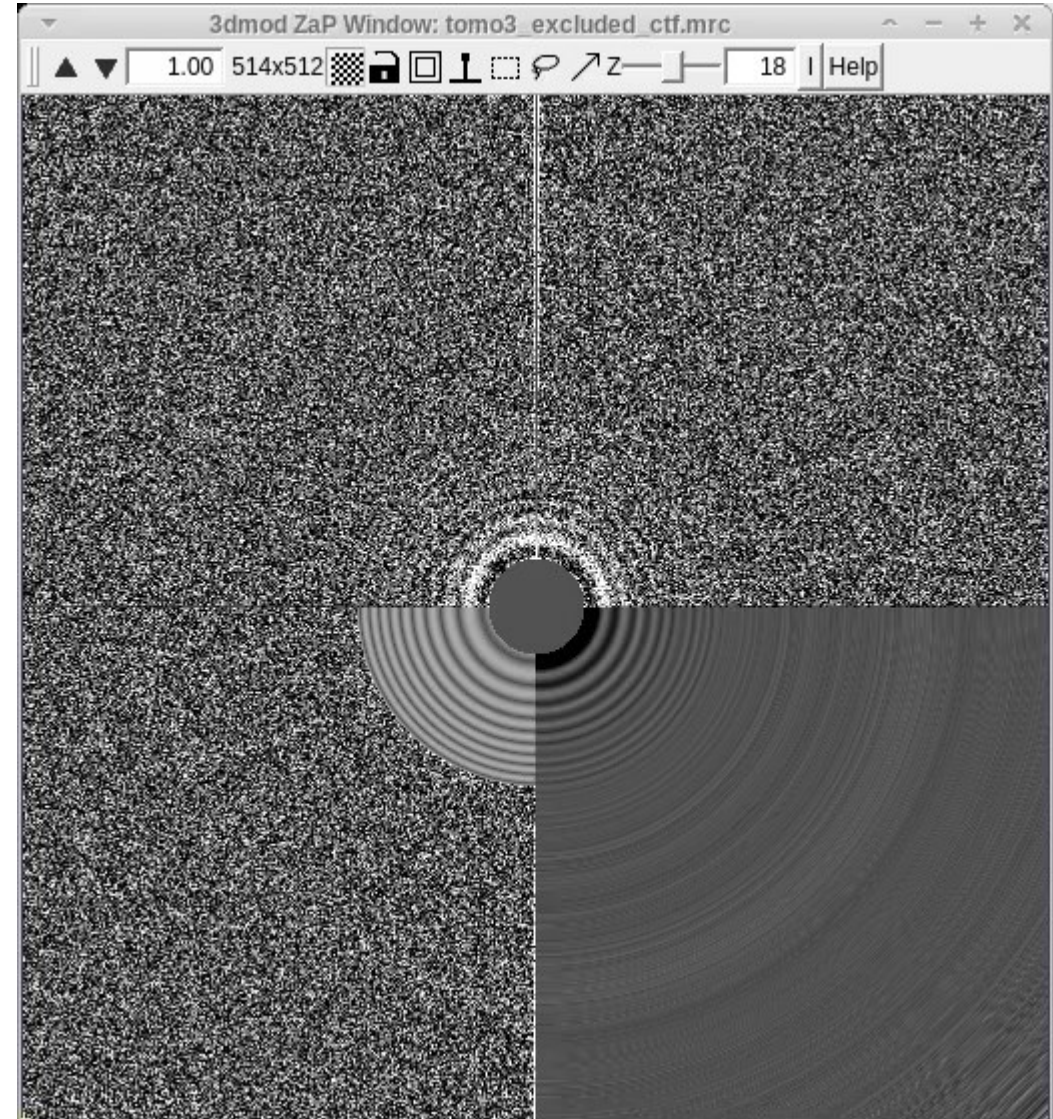


CTF Estimation

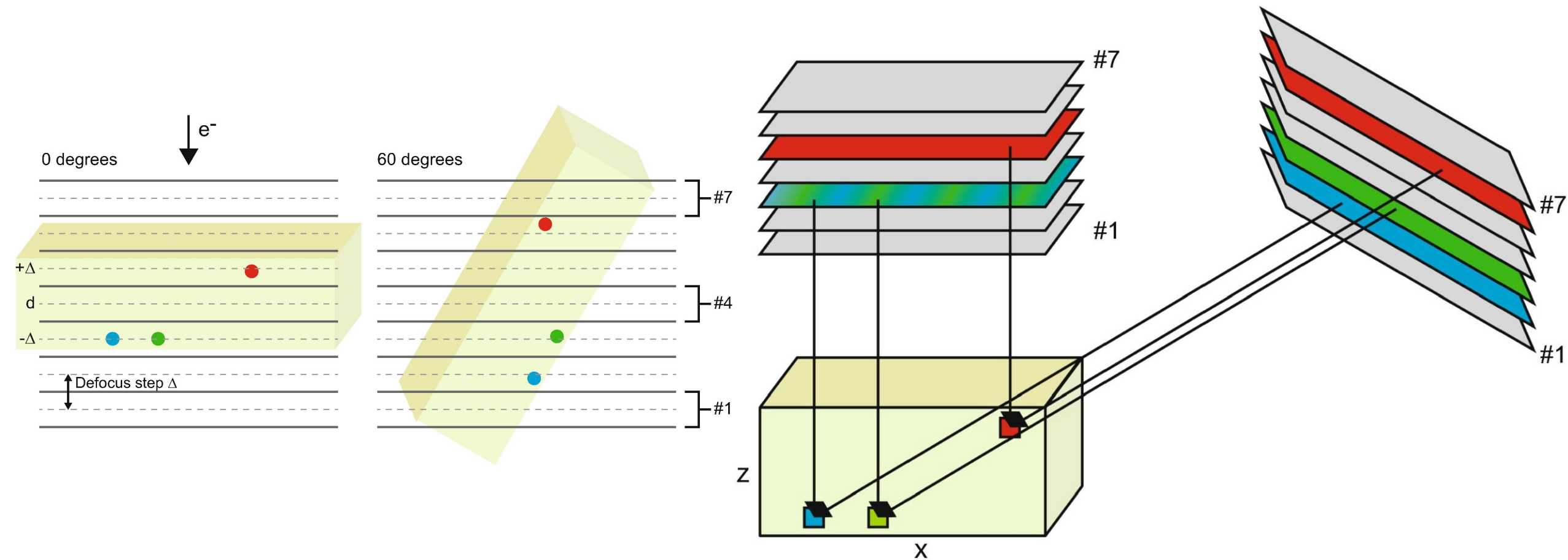
Unconstrained CTF fit



Constrained search range, constraining resolution
Gradually depending on the tilt angle



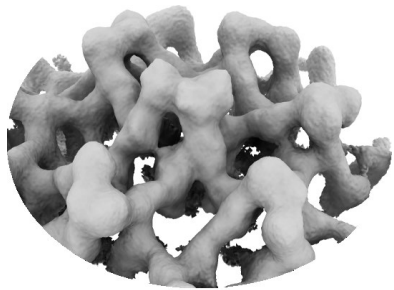
CTF correction during tomogram reconstruction



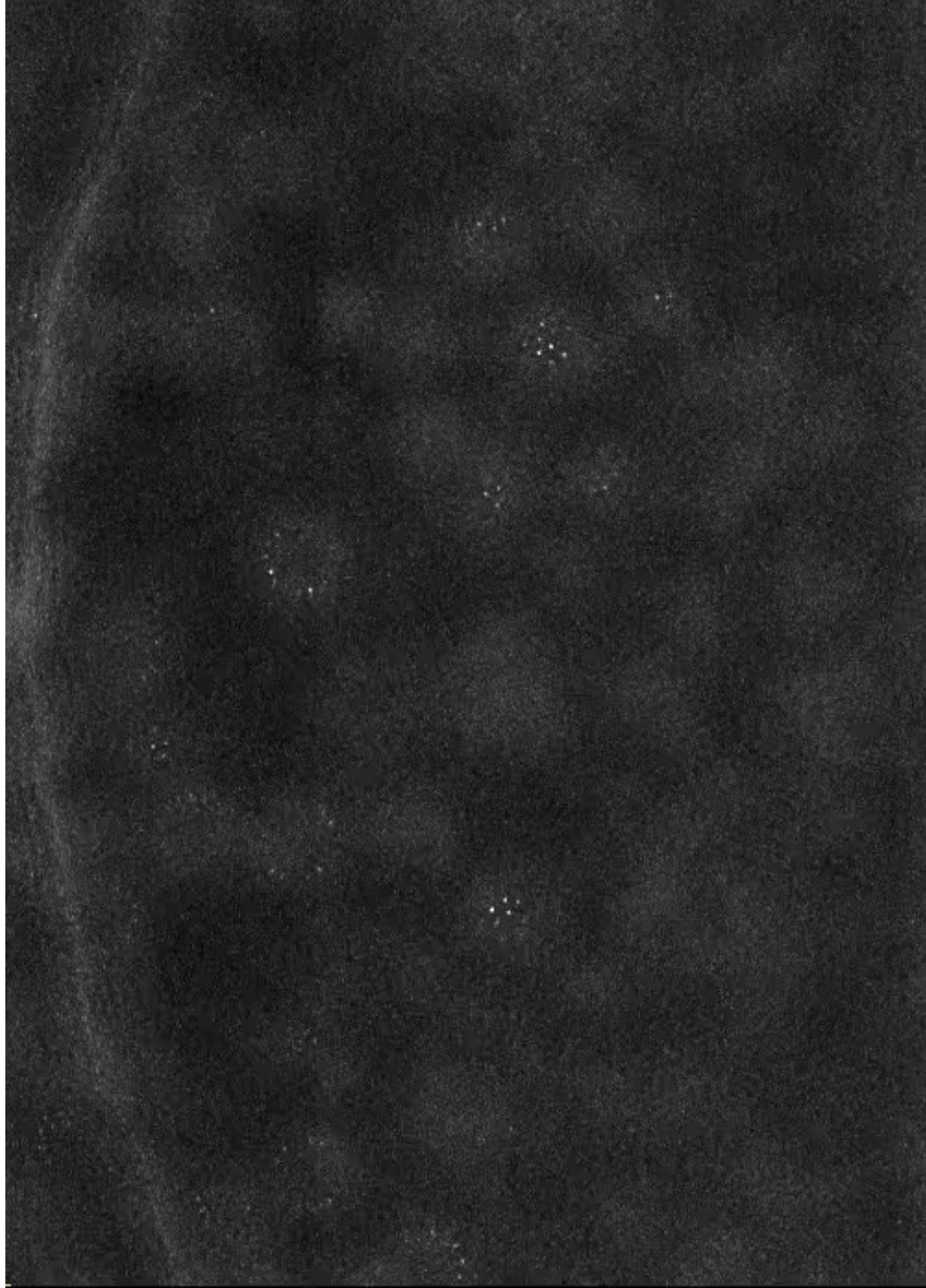
Template matching

- Hard to locate particles in 3D tomograms with “missing wedge”
- Manual picking
 - When no template is available
 - Manual curation of template matching results
- Template matching
 - Need template for matching
 - Looking for a 3D volume in a 3D volume
 - Cross-correlation methods
 - Orientational search of the template
 - Computationally expensive
 - Produce not only coordinates (X, Y, Z) but also the best fitting orientation (ϕ, θ, ψ)
 - Many false positive matches

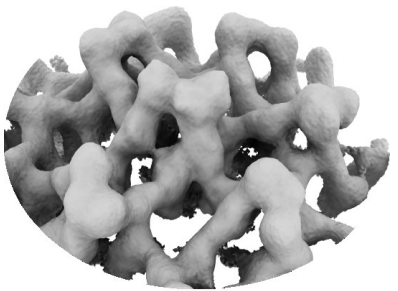
3D correlation map



template



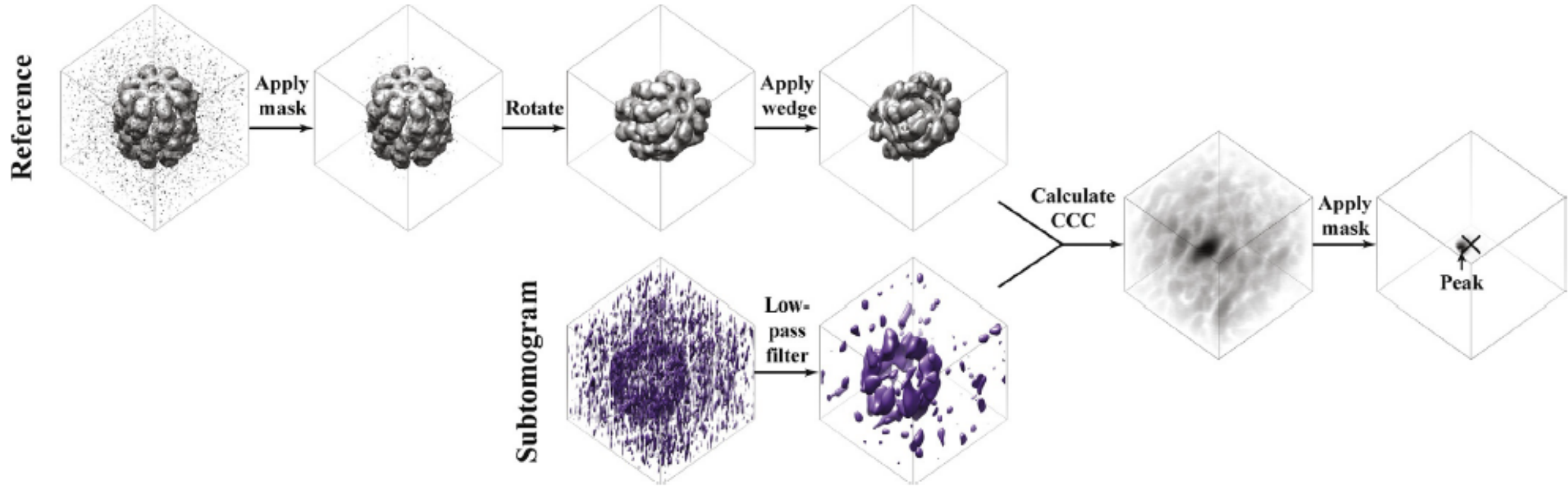
Template Matching



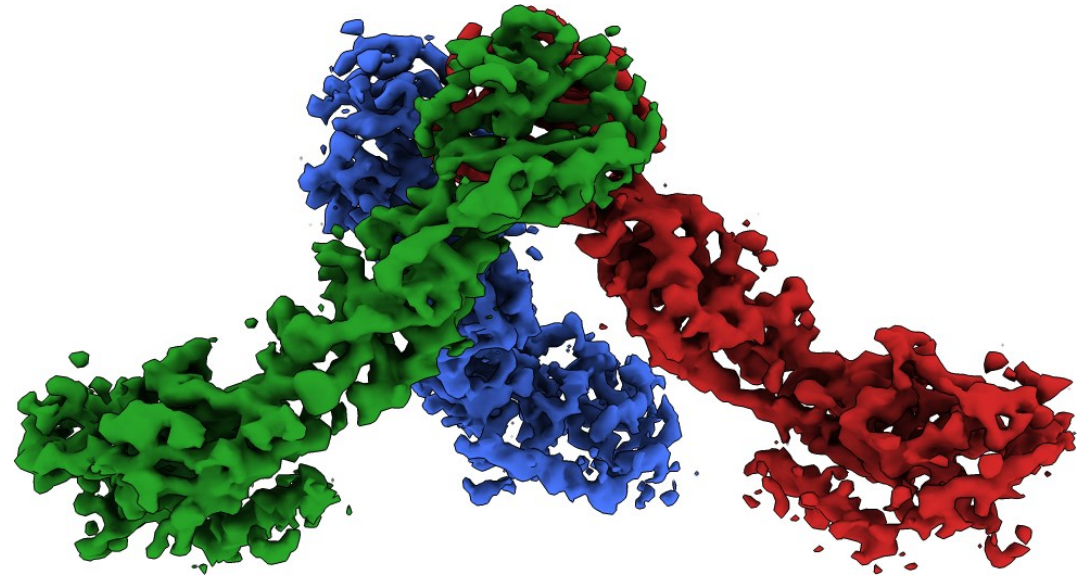
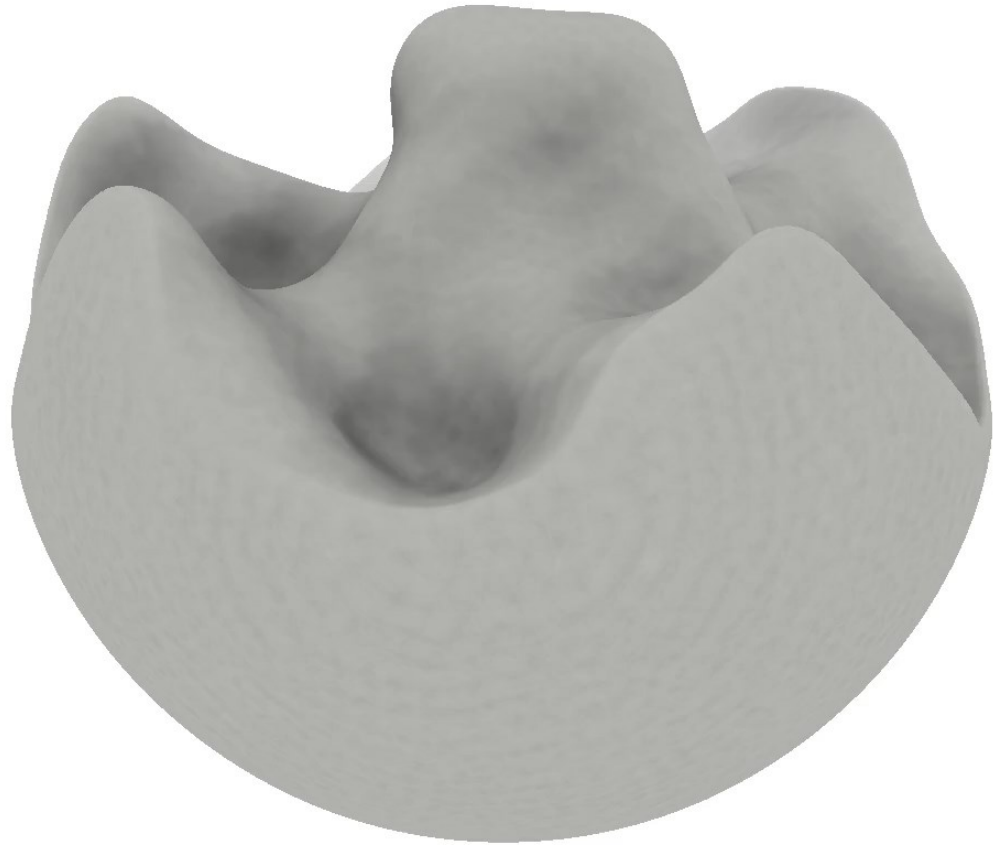
Sub-tomogram Averaging process

- Iterative process as SPA refinement
- Initial model can be generated from the data (need to be lowpass filtered)
- Computationally expensive
 - Aligning 3D volume on 3D volume
 - 3 Euler angles, 3 shifts
- Cross correlation/Maximum Likelihood methods
 - Need to compensate for the “Missing wedge”
- Speeding up calculations by gradual unbinning of the sub-tomograms
- Coarse search on heavily binned particles
- Fine (local) search on unbinned particles

Sub-tomogram Averaging process

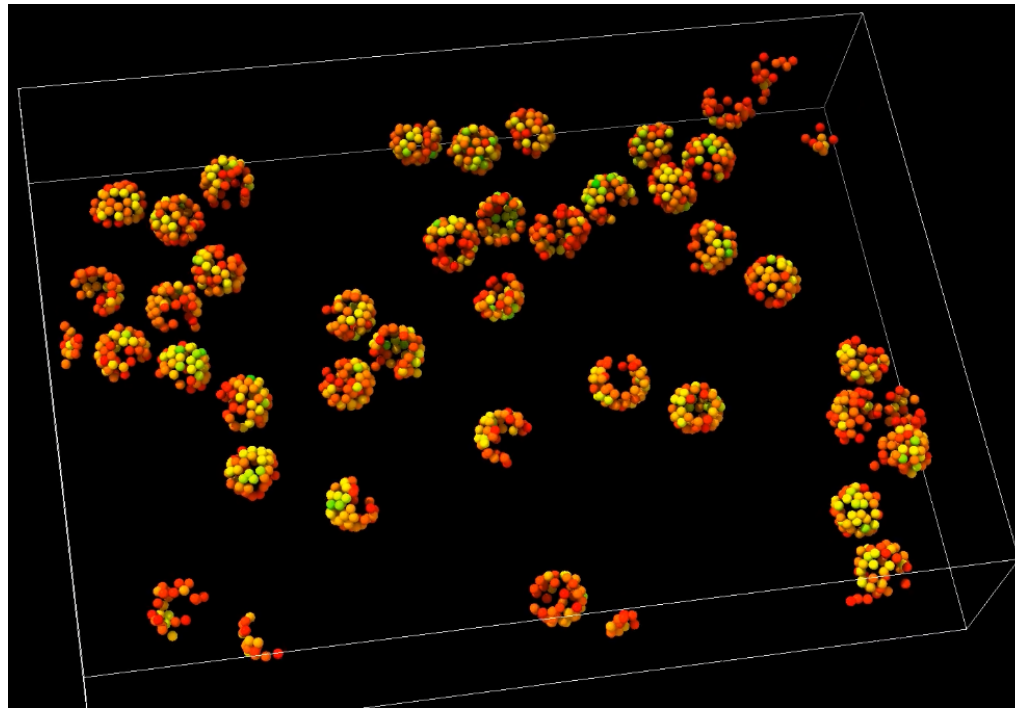


Sub-tomogram averaging – gradual refinement

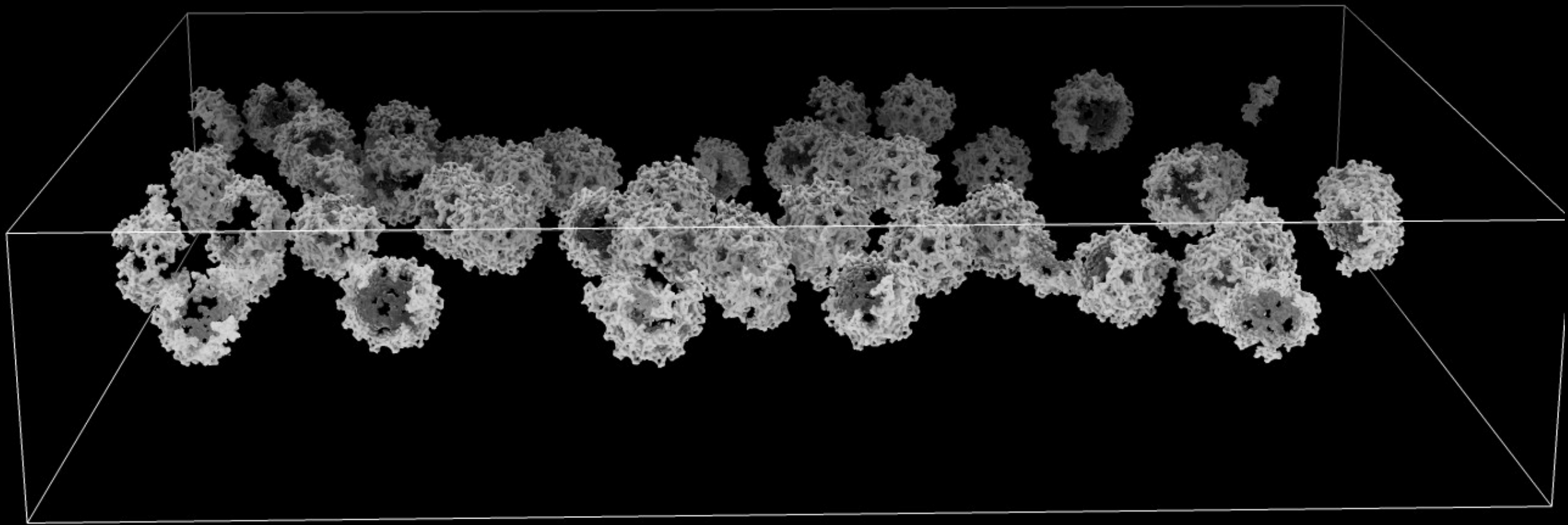


Placeback of averaged sub-tomograms

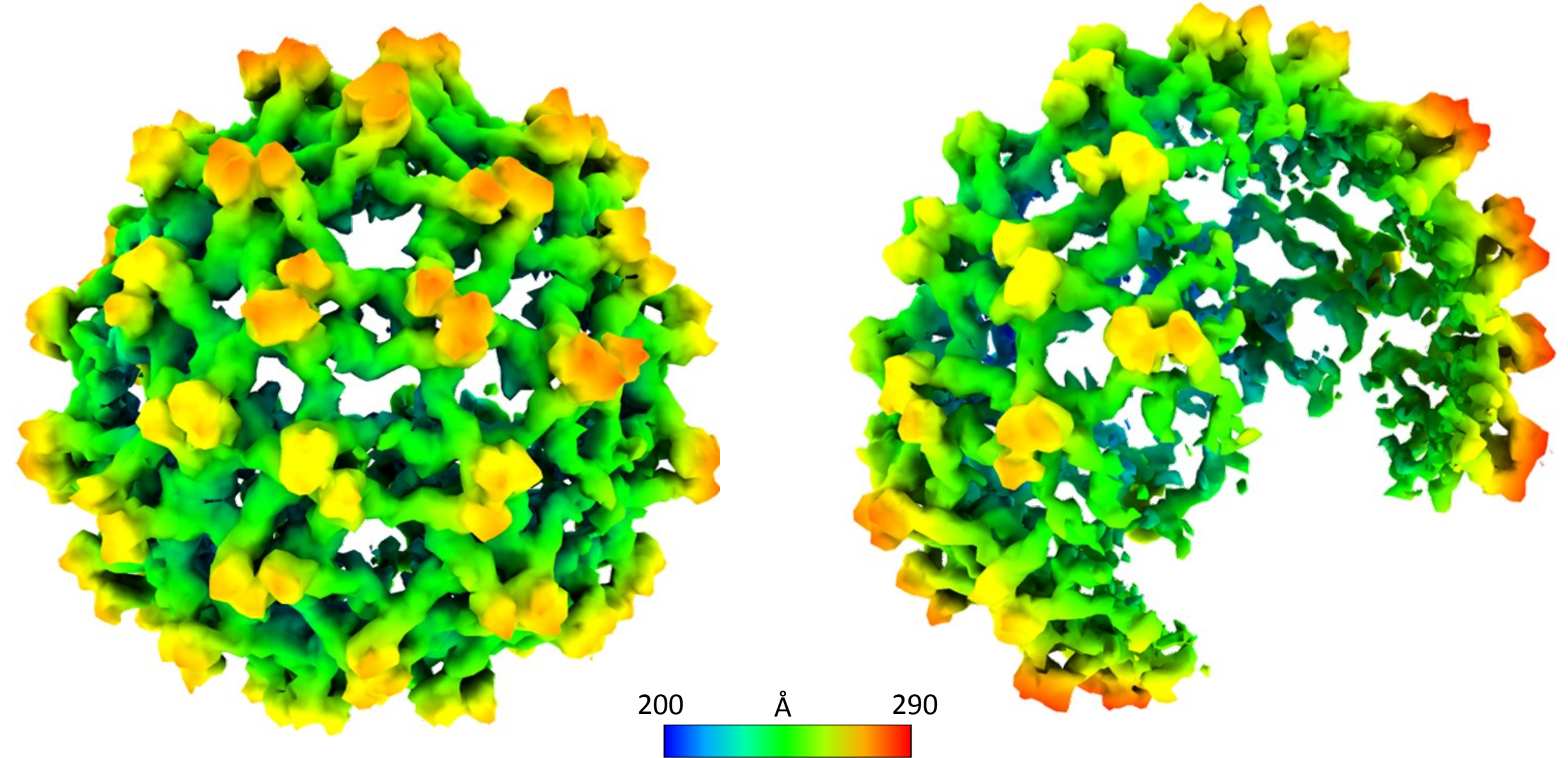
- Positions of the sub-tomograms in the tomogram is known
- After averaging the sub-tomograms have refined orientations and shifts
- Placing back the refined volume into the original tomogram
- Describes better the data in tomogram than segmentation



Placeback of averaged sub-tomograms



Selected placeback particles



Conclusion

- Electron tomography
 - Advantages / disadvantages
 - Sample preparation
 - Data acquisition (limitations)
 - Data processing
- Electron tomography future
 - Sub-tomogram averaging *in situ*
 - Speeding up data acquisition
 - Automated data processing
 - Combination of tomography and SPA
 - Correlative microscopy (combination of fluorescent and electron microscopy)

Thanks for your attention!

#teamtomo